

No. 366 March 1989

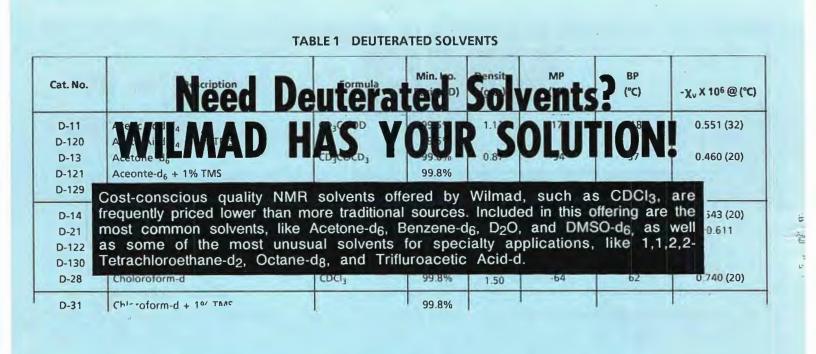
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FORTHCOMING NMR MEETINGS

San Francisco Symposium - "In Vivo Magnetic Resonance Spectroscopy II", March 31 - April 2, 1989; San Francisco, California; See Newsletter 363, 17.

30th ENC (Experimental NMR Conference), April 2-6, 1989; Asilomar Conference Center, Pacific Grove, California; Conference Chair: A. N. Garroway; Contact Ms. Judith A. Watson, ENC Conference Center, 750 Audubon, East Lansing, MI 48823; (517) 332-3667. See Newsletter <u>362</u>, 69.

11th Symposium - NMR: State of the Art and Future Directions, April 29, 1989; Dept. of Chemistry University of Rhode Island, Kingston, RI 02881; Contact: B. Sherman or R. Pothier, (401) 792-2203; See Newsletter <u>366</u>, 55.

<u>3rd Chianti Workshop on Magnetic Resonance Relaxation</u>, May 28 - June 2, 1989; San Miniato (Pisa), Italy; Contact: L. Banci, Dipartimento di Chimica Bioinorganica, Universita degli Studi di Firenze, Via Gino Capponi 7, 50121 Firenze, Italy. See Newsletter <u>362</u>, 68.

9th International Meeting on NMR Spectroscopy, Sponsored by the Royal Society of Chemistry, July 10-14, 1989; University of Warwick, Coventry, England; Contact: Dr. John F. Gibson; (01) 437-8656; See Newsletter <u>364</u>, 72.

NMR Spectroscopy In Vivo (Clinical Applications), July 10-12, 1989; Lyon France; Contact Prof. M. Amiel - see Newsletter 364, 73.

10th ISMAR Conference, July 16-21, 1989; Morzine (Haute-Savoie), France. (Note the newly announced location.); Contact: P. Servoz-Gavin, Departement de Recherche Fondamentale, Centre d'Etudes Nucleaires de Grenoble, B.P. 85X, 38041 Grenoble Cedex, France.

<u>The Society of Magnetic Resonance in Medicine - Eighth Annual Scientific Meeting and Exhibition</u>, August 12-19, 1989; Amsterdam, The Netherlands; Contact: The S.M.R.M. Business Office, 1918 University Ave., Suite 3C, Berkeley, CA 94704; (415)841-1899, FAX (415)841-2340.

Fastern Analytical Symposium, September 24 - 29, 1989; New York City; Contact: EAS, P. O. Box 633, Monchanin, DE 19710-0633; (302) 453-0785.

Additional listings of meetings, etc., are invited.



DEPARTMENT OF HEALTH & HUMAN SERVICES

Dr. Bernard L. Shapiro

TAMU NMR Newsletters

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Public Health Service

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January 18, 1989 (received 1/24/89)

Molecular Structures Using NMR and Restrained Dynamics

Dear Barry:

For some time now we have been determining the structures of peptides and small proteins in solution using the relevant 1D and 2D NMR techniques (such as HOHAHA and ROESY). During the course of these investigations we have wondered just how well these three dimensional structures are actually being determined. Do the NMR results actually lead to low energy conformations when one considers precision on the estimate of the internuclear distances?

In order to partially answer this question we have initiated two distinct lines of research. We have carried out extensive restrained (by experimentally determined distances) molecular dynamics simulations in the presence of solvent for times up to 100 psec. using many randomly generated starting structures. We find that the restraints are required to obtain acceptable low energy structures during the simulation period, and that it is necessary to explicitly include the surrounding solvent molecules.

We have also investigated the effect of digitization error on the precision in the estimate of cross peak volumes (in NOESY and ROESY) from which the restraints are derived. For typical situations in 2D NMR where a 1024 X 1024 data point matrix covers 3000-5000 Hz X 3000-5000 Hz (protons), errors can easily be as large as 100%. (Note that this error is <u>only</u> due to digitization and that instrument noise adds to the total error.) This translates to a 16 % error in the estimate of the internuclear distance and must be considered when estimating the restraint energies in the dynamics simulations. We are attempting to translate our results to the determination of an "R factor" in order to keep up with our crystallographer friends (if we have any left).

Please credit this contribution to Bob Highet's account.

Best regards,

James A. Ferretti



Kyou-hoon Han

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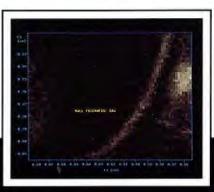
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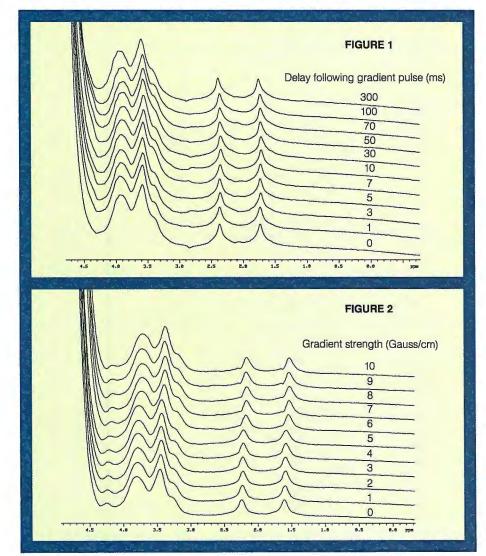


High Performance Auxiliary Gradient Coils

Dedicated RF coils, optimized for a specific application or a particular sample or both, have long been a tradition in NMR imaging as well as NMR spectroscopy. Similarly, dedicated gradient coils yield dramatic performance improvements in terms of rise and fall times, maximum gradient strength, duty cycle and eddy currents. Sophisticated eddy current compensation techniques reduce any residual spatial or temporal field variations due to eddy currents to a few hundredths of a percent, thus yielding distortion free spectra and images.

At Spectroscopy Imaging Systems we are able to obtain in-plane resolution of $20\mu \times 20\mu$ in an axial cut through an okra of 1.3 cm diameter. (See image shown on front side.) An enlargement of a portion of a seed capsule within the okra displays a wall thickness of 50μ (inset on front side). The gradient coil used to obtain this excellent performance has a diameter of 125 mm and was mounted in an Oxford Instruments 4.7 Tesla, 330 mm bore magnet without removing the standard set of gradient coils. The auxiliary gradient set is capable of generating greater than 10 Gauss/cm in all orientations using the same gradient power supply as the primary gradient coil.

The excellent control of eddy currents using the smaller gradient insert is demonstrated in Figures 1 and 2. Figure 1 shows a series of spectra of the high field region of a sample containing $[2^{-13}C]$ acetate and $[1^{-13}C]$ glucose in H_2O/D_2O . With the sample in the center of the gradient coil, a 1 second gradient pulse of 1 Gauss/cm was applied. The gradient pulse was followed by a variable delay, a 90°



RF pulse and acquisition of the resultant free induction decay. All spectra are essentially undisturbed even at delay times below 10 ms.

Figure 2 shows a typical series of spectra of the same sample at an off-center location in the magnet. A gradient pulse of 5 ms duration with an amplitude range of 0 to 10 Gauss/cm was applied, and the FID recorded at a fixed delay time of 3 ms. The sample was positioned at 22.3 mm off the center, corresponding to local gradient field of 95 kHz. All spectra are virtually undisturbed, even at 10 Gauss/cm.



January 18, 1989 (received 1/28/89)

Dr. Bernard L. Shapiro 966 Elsinore Court Palo Alto, CA 94303

Dear Barry:

SUBJECT: Obtaining Symmetrical Deuterium Spectra of Solids

Symmetrical deuterium spectra of solids are sometimes difficult to achieve. Attempts to convert an unsymmetrical spectrum into a symmetrical spectrum through software phase correction often are futile. The source of the asymmetry generally is in spectrometer tuning, not in phasing.

The asymmetry problem reveals itself through the FID if the operator is unable to adjust the receiver phase to put the signal entirely into the real channel and there is only noise in the imaginary channel. The imaginary channel can be zeroed, of course, but this leads to spectral distortion if that channel does contain part of the FID.

To get symmetrical deuterium spectra we routinely use a tuneup procedure that was developed for proton multiple-pulse nmr. We, of course, adjust the four channels of the transmitter to have equal amplitude and differ in phase by exactly 90 degrees, but we also tune out any phase glitch that may exist. The specific method was developed by Burum, Linder, and Ernst (J. Magn. Reson., 1981, 43, 463). Other tuneup techniques in the literature may also be suitable, but we have not tried them. The test sample is a little deuterium oxide in a small spherical cell. Large test cells lead to problems with rf homogeneity. The tuning generally takes only 10 or 15 minutes during setup and then doesn't have to be repeated unless the spectrometer configuration is altered.

Very truly yours,

Mark

P. Mark Henrichs Corporate Research Laboratories

PMH:



Sunbury Research Centre, Chertsey Road, Sunbury-on-Thames, Middlesex TW16 7LN

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Our ref: S/SYB/446/88

Telephone: 0932-76 2142

14th December 1988 (received 1/30/89)

Date

Dear Professor Shapiro,

NMR AT HIGH PRESSURE

In recent years a number of high pressure nmr systems have been reported (1). At BP we have a number of applications for such equipment including the study of homogeneous catalysis and organic equilibria. However, we were reluctant to commit an entire spectrometer or probe for such use. The hpnmr system described by Roe (2) involving a sapphire tube with a titanium pressure valve seemed to be well suited to our needs and therefore we set about building a similar device.

Before actually commissioning the hpnmr system we had to take into account a number of safety aspects. Obviously, once the tube was pressurised the operator must be protected from it. Therefore we designed a brass carrier with a perspex window to allow the operator to observe the sample without any danger. This carrier slots on the spinner housing at the top of the magnet. It has a removable base plate so that it can easily be used with any of our spectrometers (to date we have used it on our JEOL GX400 and FX270 and Bruker MSL100 instruments).

Our second safety consideration was for our probes! We were unhappy about "dropping" the pressurised tube into the magnet on the compressed air supply, so we designed a device to lower the tube into the magnet which detaches itself automatically from the tube once it is in place in the probe.

Having achieved the required safety standards we tested out the tube. Although it reliably held pressure, we experienced problems with spinning it as it was very heavy. In addition, we noticed a very strong pull on the tube as it approached the centre of the magnetic field, even though the titanium contained negligible amounts of iron (eddy currents?). Therefore we totally redesigned the valve so that a substantial amount of it comprised PTFE rather than titianium. After a number of modifications we now have a system which holds pressure and spins reliably (it is also considerably lighter than the original system). We now use our hpnmr setup routinely to study organic equilibria and ³⁰⁰⁻⁷ homogeneously catalysed processes at temperatures and pressures approaching those used industrially. Figure 1 shows the ³¹P spectra of a phosphine complex in a normal nmr tube and in the hpnmr tube. The resolution of the spectrum is not as good as that from the normal tube as the sample contained suspended solids. However, the results were more than adequate to study the fate of the complex during a catalytic cycle.

I hope this contribution will reinstate BP!

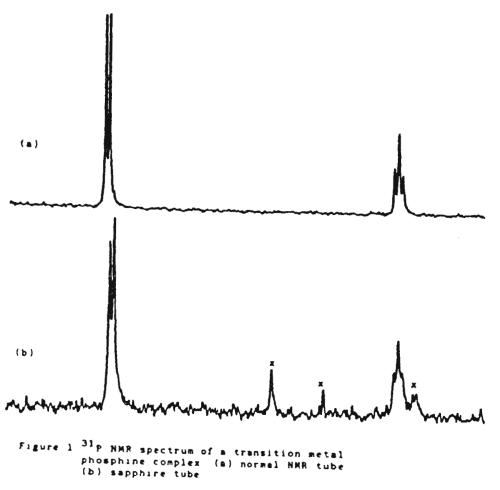
Yours sincerely

2

5- BA0

Dr J D Boyle Spectroscopy Branch

References (1) I Ando and G A Webb, Magn. Reson. in Chem. 24, 557 (1986). (2) D C Roe, J. Magn. Reson. 63, 388 (1985).



x = impurity

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DEPARTMENT OF CHEMISTRY Dr. Hellmut Eckert SANTA BARBARA. CALIFORNIA 93106 2/3/89 (received 2/11/89)

Prof. B. L. Shapiro 966 Elsinore Court Palo Alto, CA 94303

Measurement of Particle Sizes in GaP by ⁶⁹Ga Nutation NMR

Dear Prof. Shapiro:

In connection with our solid state NMR studies of colloidal semiconductors we have recently taken a look at particle size effects on solid state NMR parameters. Compared below are the ⁶⁹Ga nutation NMR spectra, obtained at 7.05 T and $\omega_1 = 33$ kHz, of (a) bulk GaP and (b) the same material pulverized overnight in a mechanical alumina grinder in an N₂ atmosphere and passed through a 100 micron sieve. The figure shows normalized frequency domain spectra arranged in order of increasing length of the excitation pulse (from 0.5 to 16µs) in 0.5µs increments. The reduction of the 90° pulse length from 7.5 (bulk) to 4.5 µs (ground) is consistent with a high degree of excitation selectivity for the central 1/2->-1/2 transition of the spin-3/2 ⁶⁹Ga nuclei in the latter material. Although the introduction of first-order quadrupolar effects in cubic solids by grinding is already mentioned in "THE BOOK", ¹ the detection by nutation NMR is more convenient than absolute signal intensity measurements, and leads to results that are easier quantifyable, especially when a distribution of quadrupole coupling constants is present. It should be possible to use the nutation effect for calibrating particle sizes in cubic powders containing nuclei with large quadrupole moments.

¹A. Abragam, Principles of Nuclear Magnetism, Clarendon Press Oxford; paperback edition (1983), p. 246-249.

Please credit this letter to Tom Gerig's account.

ground GaP. bulk GaP particle size ≤100 µm Sincerely, Hellmut Eckert Jim MacDougal

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CSI 2T Applications

Shielded Gradients and Localized Spectroscopy

Eddy current effects are the leading cause of errors and lack of consistent results in gradient localization methods. It is not surprising, then, that actively shielded gradients, which have dramatically reduced eddy currents, represent a significant technology advance for all forms of B_o gradient volume localization and spectroscopic imaging methods. The fast rise time and high gradient strength characteristics of the coil used in these experiments are also important.

Even without pre-emphasis, shielded gradients recover fast enough to obtain spectroscopic information at 1 msec or less after a strong gradient has been turned off (Fig. 1).

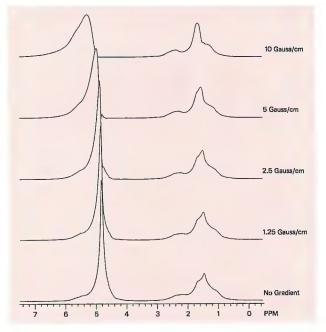


Fig. 1—Using an oil/water phantom, a 10 G/cm gradient will create a water frequency profile extending from 156 KHz to 280 KHz away from normal water resonance. Residual gradient effects of less than 0.01% (50 Hz at 10 G/cm) are observed in a spectrum acquired beginning 1 msec after a 20 msec gradient pulse. As an example, a 4DFT spectroscopic imaging technique can resolve the four frequency domains that are associated with an NMR signal from an object: x-, y-, z-spatial coordinates and chemical shift δ . The above technique can be a practical alternative to single volume localized spectroscopy. This method allows phosphorous spectra to be obtained from well-defined regions as demonstrated in the following experiment, which was carried out on a GE CSI 2T system using high-strength, shielded gradient coils (Fig. 2). The phase-encode time is kept short (on the order of the dwell-time) to minimize phase-errors in the final spectra, as well as to avoid loss of signal due to T2 decay, which is significantly short in biological phosphates.

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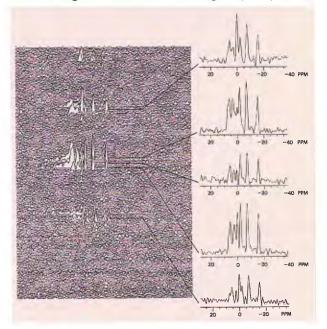


Fig. 2—Stacked plot showing 512 phosphorous spectra from 60 mm cubed region of a live rat. Each trace corresponds to 7.5 mm cubed region (voxel) from within the region of interest. The offset traces clearly show the achievable spectra and spatial resolution of the technique, as well as demonstrating localization of the liver phosphorous metabolites from that of overlying skeletal muscle. Total acquisition and processing time was two hours.



GE NMR Instruments

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DEPARTMENT OF HEALTH & HUMAN SERVICES

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Dr. Bernard L. Shapiro TAMU NMR News Letter 966. Elsinore Ct. Palo Alto, CA 94303

National Institutes of Health Bethesda, Maryland 20892 Building : 10 Room : B1D-123 (301) 496- 8140

In Vivo NMR Research Center Feb. 6,1989

Dear Dr. Shapiro:

Additional information from In Vivo Localized Proton Spectra using short echo times.

It is well known that In Vivo proton spectroscopy offers advantages with respect to sensitivity and access to different metabolites. This has been demonstrated recently for relatively large volumes in humans (1,2) and for smaller volumes in cats (4) using stimulated echoes. However, in general, only long echo times (TE \geq 50 ms) have been applied because of the problems of water (and fat) suppression. The long echo time results in a) substantial T₂ losses for some compounds, b) unwanted signal modulation in multiplets due to homonuclear coupling

and c) losses due to multiple quantum effects depending on the spin systems. Now, we are convinced that water suppression is relatively straightforward, even for short echo times, as long as the linewidth of water is determined to a large extent by homogeneous broadening (pure T₂ effects). In vivo, this necessitates a very good localization technique with minimal susceptibility and recompany offset offsets. Using the STEAM technique (2) and the

minimal susceptibility and resonance offset effects. Using the STEAM technique (3) and the shielded gradients (built by Dr. Pete Roemer of GE) on our 4.7T GE CSI instrument, we have shown that this is feasible (4). Of course, residual gradient effects should be really minimal.

With these conditions satisfied we use a combination of CHESS pulses (5) to suppress the water. Even with the inhomogeneous B_1 field of a surface coil it is possible to suppress water in this way by a factor of about 5000 or more as is shown in the spectrum of a nominal volume of 1 cm³ in the cat brain using a TE of 14 ms (the residual water signal may be used for reference purposes). The full water suppression sequence will be published soon (6).

It is evident from the spectrum that a wealth of new resonances appear with these short echo times (we think that the spectrum contains no artifacts). Interestingly, at least one new peak at low field (about 8 ppm) comes up immediately after death of the cat. We are currently investigating the assignments. We hope that, with these improvements, we are again one step closer towards exploiting the full potential of localized proton spectroscopy.

This work was performed in the NIH In Vivo NMR Research Center and will be submitted to Magnetic Resonance in Medicine.

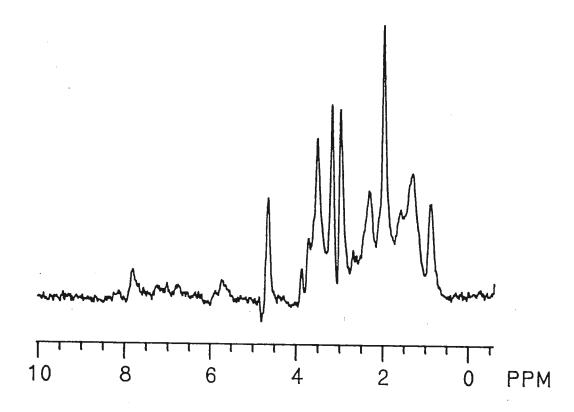
[1] J. Frahm, M.L. Gyngell, H. Bruhn, K.-D Merboldt, W. Hanicke and R. Sauter, SMRM, 7th annual meeting, 1988, p. 613. [2] P.R. Luyten, A.J.H. Marien and J.A. den Hollander, SMRM, 7th annual meeting, 1988, p.327. [3] J. Frahm, K.-D Merboldt, W. Hanicke, J. Magn. Res. 72, 502 (1987). [4] P. van Zijl, C. Moonen, J. Alger, J. Cohen, S. Chesnick, submitted to Magn. Reson. Med.[5] A. Haase, J. Frahm, W. Hanicke and D. Matthaei, Phys. Med. Biol. 30, 341 (1985). [6] C. Moonen and P. Van Zijl, to be published.

Yours Sincerely,

Chrit Moonen, BEIB, DRS



Peter van Zijl, NCI



Proton spectrum of cat brain at 4.7 T. Nominal volume 1 cm³; TE = 14 ms; TM = 50 ms. Total acquisition time 10 minutes (400 scans). Only exponential broadening and FT was applied for signal processing. The same surface coil (o.d. 6 cm) was used for transmit and receive. No surgery was performed on the cat. Some surface fat may have been detected in this particular example.

POSTDOCTORAL POSITION - PHYSIOLOGICAL NMR

A postdoctoral position is available immediately in the Biomedical NMR Center of the University of Arkansas for Medical Sciences. The ideal candidate should have a Ph.D. in a basic science and previous experience in physiological applications of NMR. The laboratory has a General Electric CSI-4.7T/33cm imaging/spectroscopy system, a GN-300WB high resolution NMR spectrometer and liberal access to a GE Signa clinical MRI system with spectroscopy. The laboratory has basic and clinical research projects in MR spectroscopy and imaging of 31 P, 1 H, 19 F, and 7 Li both <u>in vivo and in vitro</u>. Period is one year, renewable by mutual agreement. Salary is 23,000/yr. Interested individuals should send a resume and names of three references to:

Richard A. Komoroski Ph.D. Director, NMR Laboratory Slot # 582 University of Arkansas for Medical Sciences 4301 West Markham Little Rock, AR 72205

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> Dr Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303, USA

Fcbruary 2nd 1989 (received 2/13/89)

GRAPH THEORY IN AUTOMATED ANALYSIS OF Z-COSY SPECTRA

Dear Dr Shapiro,

Over the last few years, we have attempted to improve algorithms for automated analysis of 2D spectra. We noticed some time ago that it might be useful to borrow some concepts from graph theory, but we hesitated to do so for fcar of appearing too intellectual. Actually, we don't really feel a need for using any of the stunning theorems of graph theory (which saves us the trouble of trying to understand the proofs), but we like the semantics. Expressions such as 'nodes' and 'edges' sound so much better than the old-fashioned terminology of 'nuclei' and 'couplings'! Groups of magnetically equivalent nuclei are now called 'supernodes'. Who can resist the temptation of such a charming language? Actually, graphs provide an elegant description of the relationships between molecular structure and 2D NMR spectra.

Chemists routinely represent the structure of molecules by graphs (see Fig.1a). It is like Monsieur Jourdain who discovered to his amazement that he could speak in prose. To discuss ¹H NMR spectra, it turns out to be more suitable to use another type of graph that we call *global coupling network* (see Fig.1b). The nodes represent the chemical shifts of the protons, the edges stand for resolved scalar couplings between spins. Groups of magnetically equivalent spins, such as the three methyl protons symbolically represented by [3], can be fused into a supernode.

A global coupling network $G(\Omega, J)$ of nodes Ω and edges J can be subdivided into subgraphs $F^{kl}(\Omega', J')$ called fragments (Fig. 1c). A fragment consists of two active nodes Ω_k and Ω_l (chemical shifts of the active spins), their mutual active coupling J_{kl} and all passive nodes Ω_i that are connected to one or to both of the active nodes. A global coupling network can be subdivided into as many fragments as there are edges in the network. Graphically a fragment is drawn as in Fig.1c with the following conventions: active nodes are represented by ellipses, passive nodes by circles or by squares, depending on whether they are connected to only one or to both active nodes. Degenerate couplings are labelled with double cross-bars.

The cross-peaks in Fig.1d, extracted from an experimental z-filtered COSY spectrum, may be regarded as a 'mapping' of the fragments in Fig.1c onto the spectral domain. In fact, it is always possible to deduce the structure of a 2D spectrum from the molecular structure by following the path (a) \rightarrow (b) \rightarrow (c) \rightarrow (d) in Fig.1. The aim of automated analysis is obviously to derive the molecular structure by following the inverse path (d) \rightarrow (c) \rightarrow (b) \rightarrow (a). The analysis of individual cross-peaks is now sufficiently advanced so that one can get reasonable proposals for fragments. Assembling these into a global network turns out to be a more demanding task, bearing in mind that many of the fragments that are found may actually be misleading. In the language of graph theory, the problem amounts to deriving the supergraph G from the knowledge of the subgraphs F^{kl} . Although we have not found a completely fool-proof solution yet, we derive great pleasure from the fact that our difficulties can be described in noble terms.

Yours sincerely,

Peter Pfändler

Geollicy Baledon

Geoffrey Bodenhausen



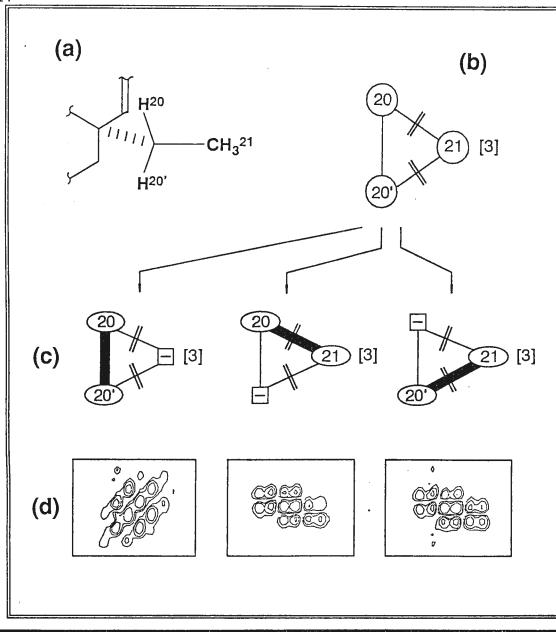


Fig.1 : (a) Graph describing part of the molecular structure of vinblastine. (b) Global coupling network of the protons H^{20} , H^{20} and the three H^{21} protons of the methyl group.

(c) Fragments that
can be extracted
from the network.
(d) Experimental
cross-peak multiplets
from a z-COSY spectrum of vinblastine.

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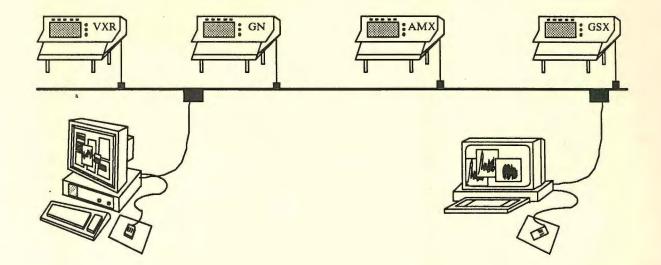
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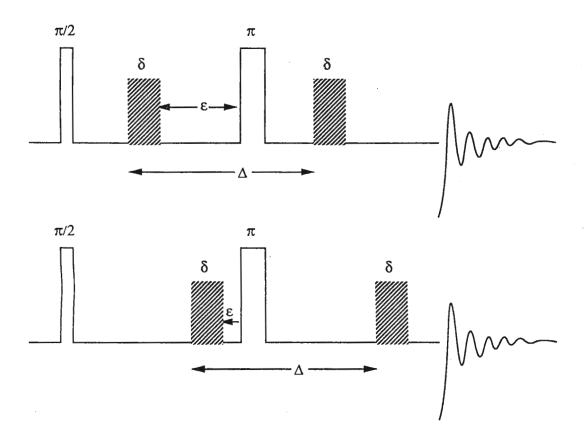
Prof. B.L. Shapiro TAMU NMR Newsletter 966 Elsinore Court PALO ALTO CALIFORNIA 94303 USA

TITLE: High Resolution PFG Diffusion Measurements in Cells

Dear Barry,

We have previously measured the relaxation rate of $[2, 1^{3}C]$ glycine to estimate the intracellular viscosity of the cytoplasm of human red cells [1,2]. A more direct approach to the problem is to use the pulsed field gradient (PFG) NMR experiment. We have recently met with success with this experiment after about 3 years of developing a system for our Varian XL/VXR 400 wide-bore (89 mm) spectrometer. The main developments which have been made are: (1) the anodized aluminium housing of the 30-105 MHz broad-band probe has been replaced by aluminium tube that extends only to the partition below the coil region; (2) we use a Maxwell pair (a pair of oppositely wound) solenoidal coils on a Perspex former which is attached to the outside of the glass-Dewar that supports the r.f. coils ; (3) the probe housing around the coils, and which supports the lower end of the spinner assembly, is made of Perspex; (4) an earth wire extends from the aluminium housing to a ring of aluminium which makes contact with the upper spinner tube; (5) the cables outside the magnet carrying the field gradient currents are all r.f.-shielded with copper braid which is earthed to the magnet; (6) the leads to the gradient coils in the probe are shielded by being in 4 mm Pyrotenax (copper coated 2-wire cable); (7) the fast-switching linear amplifier is home built and receives its logic pulses from the spectrometer via an optic coupler. Some of our first results obtained with the apparatus are about to appear in the refereed literature.

We have recently had cause to evaluate PFG diffusion apparatus from two leading manufacturers and in the course of those discussions it was necessary for us to define a "key" experiment which could be used to assess the quality of the apparatus. The experiment is the classical Stejskal and Tanner [3] one in which a linear field gradient pulse is applied in each of the two time intervals of a spin-echo r.f.-pulse sequence. For our test we suggest, for the common nuclei (1H, 13C, 31P), a total echo time of 200 ms, a field gradient pulse of around 20 Gcm⁻¹ of duration (δ) 5 ms and a time interval between the leading edges of the gradient pulses (Δ) of 100 ms. The time interval between the trailing side of the first gradient pulse and the start of the π r.f.-pulse is denoted ε in the figure below. In evaluating the PFG equipment we recommend holding δ and Δ constant and diminishing ε from ~50 ms to as small a value as possible. For a properly functioning apparatus the Fourier transform of the spin-echo FID is a spectrum whose phase parameters and amplitude are independent of ε . For our home-built apparatus this holds true down to ε values of 7 ms.



It is worth noting that our apparatus does not involve the use of pre-emphasis on the ~ 20 Gcm⁻¹ gradient pulses; this is probably the result of having a wide-bore magnet. We would like to hear of the experiences of any other research group with obtaining high resolution PFG spectra using probe-solute concentrations in the mM range.

Yours sincerely,

PHILIP W. KUCHEL

Philip W. Kuld

w.s. Price

(Se Chopman

B.E. CHAPMAN

Z.H. Endre, E.B. Chapman and P.W. Kuchel, Biochem. J. <u>216</u>, 655, 1983
 Z.H. Endre and P.W. Kuchel, Biophys. Chem. <u>24</u>, 337, 1986
 E.O. Stejskal and J.E. Tanner, J. Chem. Phys. <u>42</u>, 288, 1965

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הפקולטה למדעים מרוייקים ע״ש ריימונד ובברלי סאקלר בית הספר לכימיה

Dr. Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303 USA

Dear Dr. Shapiro:

January 18, 1989. (received 1/26/89)

¹H - ³¹P CORRELATED 2D NMR SPECTROSCOPY OF INTACT ORGANS.

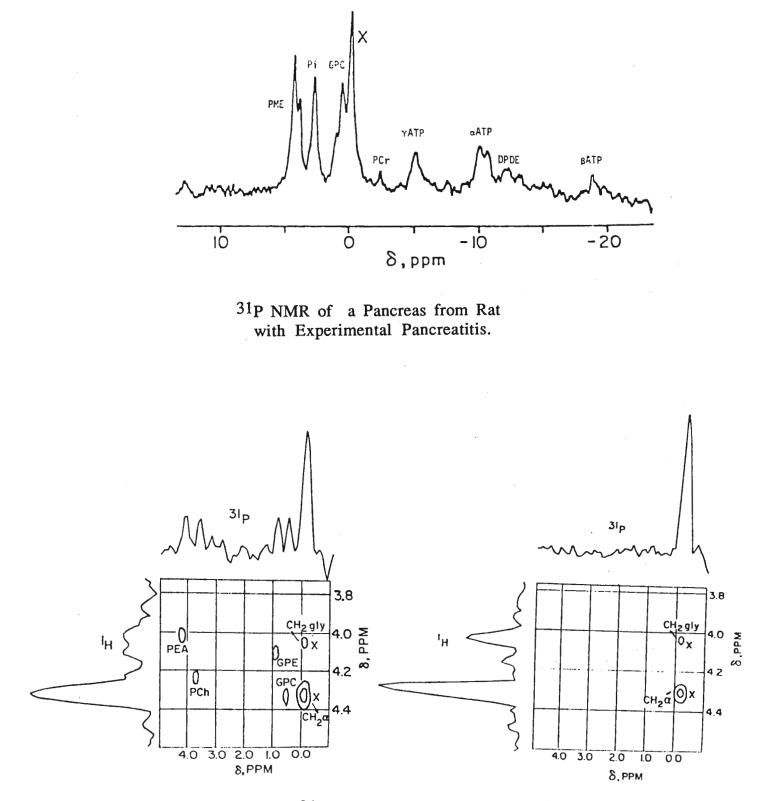
The assignment of 31P NMR signals in intact organs has been traditionally performed by the analysis of the spectra of tissues extracts. There are however cases where this approach does not lead to definite identification. In our previous ³¹P NMR studies of taurocholate induced experimental pancreatitis a new transient signal appeared at -0.18 ppm (see Fig. 1). It was suggested that this compound can be a useful diagnostic and prognostic marker, and would aid in studying the basic pathophysiologic processes of the disease. Attempts for assignment of that peak by comparing the chemical shift to genuine compounds, and by using TLC and columns chromatographic methods of PCA extracts were unsuccessful. A ¹H-³¹P correlated 2D NMR spectroscopy of the intact pancreas (Fig. 2a) gave the unequivocal assignment of the signal. In this technique, only those protons that are spin-spin coupled to ³¹P nuclei are obtained. Thus the proton spectra are greatly simplified, the strong interforing signal of the water is eliminated, and it enables precise assignment of the phosphorous signals by correlating them to the proton chemical shifts of the groups to which they are coupled. The new phosphorous peak in the discased pancreas correlated with two proton signals with chemical shifts of the choline αCH_2 and glycero CH₂ of lecithin. The compound was identified as taurocholate-lecithin complex. A 2D map of prepared taurocholate-lecithin solution (Fig. 2b) was identical. A signal with similar chemical shift was found in the PCA extracts of diseased pancreases. However, the 2D map of the extracts was completely different, and the signal must originated from a different chemical compound.

We recently performed ${}^{1}H^{-3}P$ correlated 2D NMR studies of experimental pancreatic carcinoma. The ${}^{3}P$ spectrum is dominated by the phosphomonoester peaks. 2D measurments demonstrated that this region is governed by phosphocholine (PC) and phosphoethanolamine (PEA), as well as other phosphorous compounds that overlapped PC and PEA in the ${}^{3}P$ spectrum but not in the ${}^{1}H$ dimension. Thus, this technique can provide a powerful tool for studying biochemical and metabolic processes in intact organs.

Sincerely yours,

Tammar Kushnir Ofer Kaplan Nadir Askenasy Gil Navon T. Kushyir Okplan Asll Gil Navin

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2D 1_H - 31_P NMR Correlation Spectra of: a. Intact Pancreas from a Diseased Rat. b. Lecithin-Taurochlate Complex.

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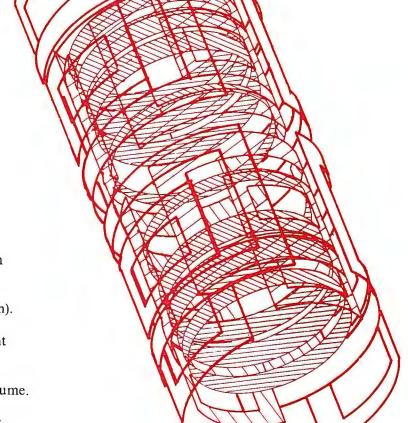
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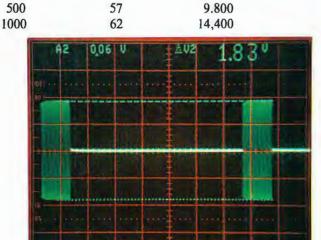
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University of Warwick Coventry CV4 7AL Department of Physics Tel: 523523 Ext. 2403 DR. RAY DUPREE

18 January 1989 (received 2/1/89)

Dr B L Shapiro 966 Elsinore Court Palo Alto California 94303 USA

Dear Barry

OH GROUPS IN COAL TARS

One challenge we have recently faced is that of identifying and quantifying -OH groups (phenol, alcohols, carboxylic acids) in coal tars. These tars are, of course, very complex mixtures. Following Dereppe and Parboo¹, we derivatise the -OH groups fairly quantitatively, using hexamethyldisilazane, and then take the ²⁹Si DEPT or INEPT spectrum of the O-SiMe₃ groups. The figure shows one example, from a high-rank bituminous coal.

Obviously we started by recording the shifts for the derivatives of single known compounds. These fall rather nicely into separated groups. Also, within a group, they correlate fairly linearly with the pK_a of the -OH group, unless there is an obvious ortho-interference. We are thus able to assign the resonances of unknown materials with some confidence. We have also shown that the peak areas correspond with known composition ratios in test samples.

The figure shows that many individual resonances can be resolved, even in the polyaromatic phenol region around 22 p.p.m.. The same remains largely true for source-fuels ranging from wood through to anthracite. We can thus trace the fate of individual compounds as coalification proceeds. Many of the changes are as expected. Wood tar is rich in aliphatic alcohols, but these have almost gone in lignites. Decarboxylation is complete by the sub-bituminous stage, and then the phenol balance swings somewhat towards polyaromatic phenols.

However, we have one unexpected general observation. In a few cases, such as with α - and β -naphthol, we can see a clear trend towards the thermodynamically favoured isomer as coalification proceeds. Another example is a trend from Ar(alkyl) to Ar(polymethyl). We are now assembling further evidence to support this detailed view of coalification as a multi-million year move towards thermodynamic equilibrium.

Yours sincerely

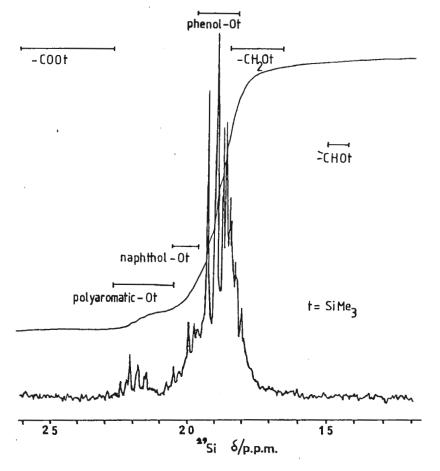
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Giles Ratcliffe

¹ Dereppe, J.M. and Parboo, B. <u>Anal. Chem. 58</u>, 2641 (1986)



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(received 2/1/89) 24 January 1989

Dear Prof. Shapiro

Homonuclear Hartman-Hahn (HOHAHA or TOCSY) spectra have proved to be of considerable value in identifying spin systems in proton spectra of proteins. Recently Feng & Roder [1] reported that the HOHAHA spectrum of an exchanging system (a mixture of reduced and oxidised cytochromes) contains cross-peaks arising from the exchange process. This arises because both coherent and incoherent transfer of magnetization occur during the spin-lock period We have observed the same effect in the

commonly-studied situation of a ligand binding to a protein, in this case the inhibitor pyrimethamine (in slow exchange) to dihydrofolate reductase. As would be expected, rotation about the bond linking the phenyl and pyrimidine rings is highly restricted, and separate signals are observed for all four protons of the chlorophenyl ring of the bound inhibitor (2' 5.87; 3' 7.07; 5' 7.93; 6' 7.65 ppm, as determined by 2D exchange spectra). The cross-peaks between the two pairs of protons on either side of the ring are shown in the COSY spectrum (fig.2). In the HOHAHA spectrum (fig.1) these scalar coupled correlations are seen again (labelled J). In addition, however, cross-peaks are seen for both direct exchange (eg 2'bound \leftrightarrow 2'free; labelled D) and relayed exchange (eg 2'bound \leftrightarrow 2'free \leftrightarrow 3'free; labelled R). The relative intensities of these cross-peaks are a function of the spin-lock time, here 50 msec (this is too short to observe effects due to long range coupling across the ring).

An important feature of this experiment is that the concentration of the free inhibitor in the sample was very low - only about 1/50th that of the enzymeinhibitor complex. This small amount of free ligand is nonetheless enough to have a considerable effect on both HOHAHA and NOESY spectra. in this case, where all the protons of the bound ligand had been assigned, interpretation was not too difficult, but we may not always be so lucky.

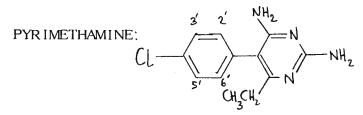
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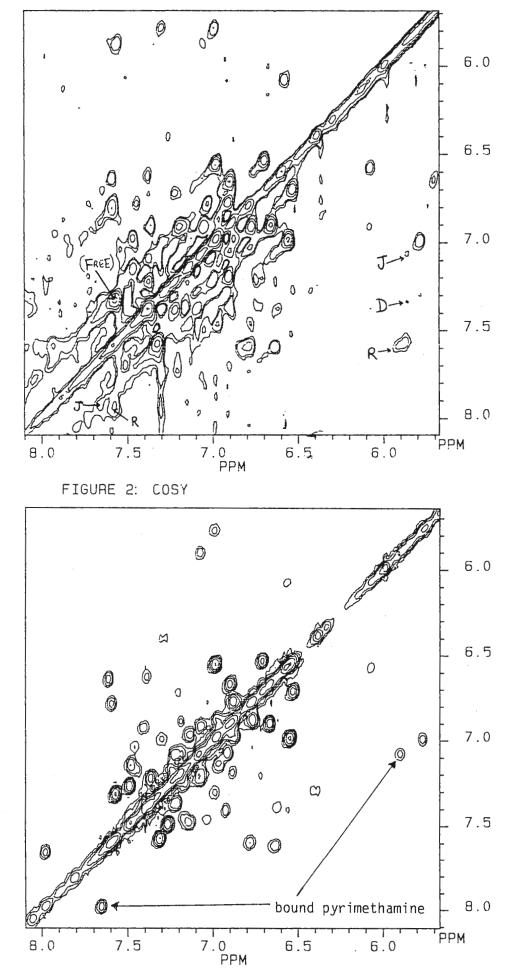
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Ref. [1] Y.Feng & H.Roder, J.Magn.Reson., 1988, 78, 597.





Prof. G. C. K. Roberts Dr. L. Y. Lian



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Prof. B.L. Shapiro TAMU NMR Newsletters 966 Elsinore Court Palo Alto CA 94303 Predicting missing or erroneous data points by linear prediction or ... the revisited story of CASSANDRA (title too long; shorter one provided for table of contents, by BLS) (received 2/15/89)

Dear Barry,

In spite of its rather primitive nature, Fourier transformation is still widely used in NMR for obtaining frequency-domain spectra. However, there is some magic involved in this simple and fast algorithm, so that everybody just feign ignorance on its pitfalls or limitations... until inconvenient artefacts show up.

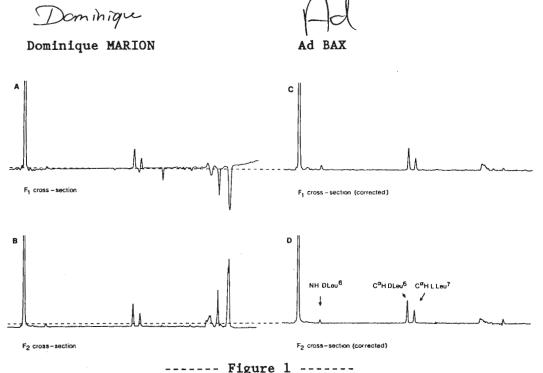
A naive spectroscopist may believe that the Cooley-Tukey algorithm (1) has been correctly implemented by the spectrometer manufacturer; but as any belief, this should be re-examined at least once. For example, are the first and last data points suitably scaled before FT (2), does the FT introduce a bias in the phase of the signal (a cosine-modulated signal should lead to a purely absorptive lineshape), does an inverse FT restore the time-domain signal at its original scaling?

As a result of the sampling theorem (3), the FT also plays strange tricks at the Nyquist frequency, especially if one is not aware of the type of FT (either *real* (4) or *complex*) employed. The striking observation, that NMR signals usually fold differently on the two sides of the Atlantic, is in no way related to the continental drift and remains beyond comprehension... until a correlation is made with the leading manufacturer on each side. Nobody runs single channel detection spectra anymore, and thus the term quadrature detection is generally useless if the sampling mode (simultaneous or sequential) is not specified. In fact, the folding pattern at the Nyquist frequency is only related to the sampling mode, which then implies the use of a given type of FT.

Baseline distortion is another devil of the FT pantheon. Without much regard to its physical origin, spectroscopists have performed cosmetic baseline corrections of one-dimensional spectra essentially in the frequency-domain. Techniques ranging from tedious adjustement on a flickering screen to highly sophisticated optimization routines have been used in the past for 1D NMR spectra; however, none of these are very suitable for 2D NMR. Optimization routines, whose efficiency is known to depend upon the starting point, often fail for a number of slices in a crowded 2D correlation map and nobody in our group is willing to spend weekends in a dark sub-basement correcting manually slices of high-resolution 2D spectra. Furthermore, mathematical models used for frequency-domain correction were obviously chosen for programming convenience (polynomial or spline functions) rather than based on the physical origin of the distortion.

Two major causes of baseline distortion are the following; the sampling is not initiated at time t=0 because of the duration of the pulses (leading to a sizeable frequency-dependent phase correction) and a couple of points at the beginning of the FID are sampled incorrectly (due to the time response of the analog filter (5)). These distortions, encountered in the F_1 and F_2 dimensions of 2D spectra, can be eliminated in the time-domain, if the missing or distorted early points can be restored from the later "error-free" points. In view of the etymological origin of its name, linear prediction is the suitable technique for extrapolating the future of a time series from its past and conversely. Using the fast algorithm developed by Burg, we were able to reconstruct the early data points of the FID and obtain almost perfect spectra using conventional FT. As compared to the regular use of LP for spectral estimation, our method (LP extrapolation + FT) is less demanding in computer time and is thus applicable for routine processing of 2D NMR spectra. Fig. 1 compares F_1 and F_2 slices for untreated and LP-corrected 2D data sets showing a dramatic improvement upon use of LP. By using the LP algorithm in conjunction with backward and forward FT, the calculation time needed for processing a typical 2D NOESY set is only about 15 min on a SUN-4. More details will be presented elsewhere (6).

Fig. 1 demonstrates that extrapolation using linear prediction is able to predict missing or corrupted data points in a reliable manner, leading to almost <u>unbelievable</u> spectra. Thus a suitable name for this method is *CASSANDRA* (7), a name that should be thought of as a mythological reference rather than as one more tortuous and mysterious acronym.



- ----- Figure 1 ------
- (1) J.W. Cooley & J.W. Tukey (1965) Maths Comput. 19, 297
- (2) G. Otting, H. Widmer, G. Wagner & K. Wüthrich (1986) J. Magn. Reson. 66, 187
- (3) R.R. Ernst, G. Bodenhausen & A. Wokaun (1987) Principles of NMR in one and two dimensions p. 104
- (4) Additional baseline distortions may be encountered when using a real FT: see D. Marion & A. Bax (1988) J. Magn. Reson <u>79</u>, 352
- (5) D.I. Hoult, C.-N. Chen, H. Eden & M. Eden (1983) J. Magn. Reson. <u>51</u>, 110
- (6) D. Marion & A. Bax J. Magn. Reson. (in press June 89)
- (7) Homer The Iliad Book XIII (Date unknown) and Aeschylus Agamemnon (5th century B.C.)

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Professor Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303 January 9, 1989 (received 1/26/89)

"NMR Spectroscopy and Recovery of a Surgically Modified Animal"

Dear Professor Shapiro:

In our recent in-vivo NMR studies, we have used a home-built surface coil probe to examine rat liver toxicity. This probe was designed for a Varian XL-400 vertical wide bore NMR spectrometer and tuned to ³¹P at 161.9 MHz. In performing these experiments, it was necessary to surgically expose the liver in order to eliminate signals from muscle. A phosphorous NMR spectrum of muscle, obtained when the surface coil is placed directly over the skin of the rat's abdomen, is shown in Figure 1.

The surgical procedure, necessary to insure that the phosphate signals were predominately from the liver, required the removal of the abdominal musculature. The superficial skin flaps were then reflected and sutured laterally. The absence of the phosphocreatine peak in the ³¹P spectrum (Figure 2) gave good indication that we were focussed on the liver. These experiments, however, required that the animal be sacrificed immediately following the NMR scan, making it impossible to follow the time course of a toxin in a single animal.

We now report a surgical procedure which not only allows ³¹P NMR spectra to be obtained from the liver without interference from skin and muscle but also permits recovery and survival of the animal. The procedure involves the removal of the abdominal muscle overlying the liver and surgical implantation of a Mersilene mesh (Ethicon, Somerville, N.J.) to the remaining abdominal musculature. Following suturing of the skin flaps back to their previous anatomic position, the animals were allowed to recover from the Ketamine induced anesthesia. Three days post surgery, phosphorous spectra were taken through the skin of the underlying liver. The results (Figure 3) show an absence of the phosphocreatine peak indicating no observable contamination from skin or muscle. The animals survived for 6 weeks post surgery and were finally sacrificed. Muscle regeneration was observed after four weeks.

The implantation of the mesh and the successful recovery of the animals allows NMR studies of rat liver metabolism to be carried out over an extended time frame on a single animal. To the best of our knowledge, the implantation of the

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Mersiline mesh for the purpose of NMR studies using a surface coil probe is the first of its kind and may prove useful for drug studies in which liver metabolism is monitored.

Sincerely,

Jeff Platchok

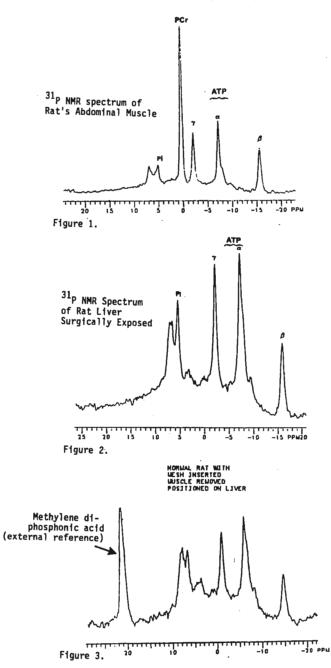
Jeff Plutchok

nina C. Gonnella

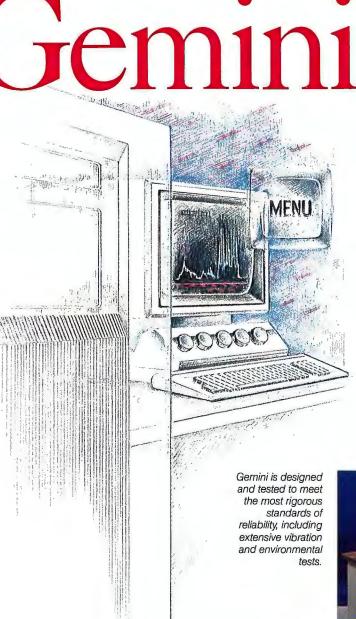
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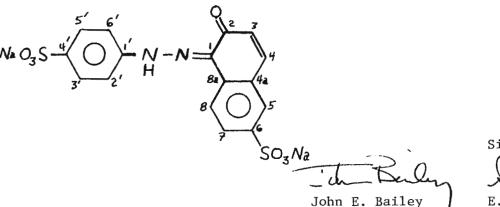
Dr. Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Ct. Palo Alto, CA 94303

• Determination of Indirect C-H Connectivities by the FLOCK Sequence

Dear Barry,

The assignment of quaternary carbons in aromatic compounds is particularly difficult because "model" compounds cannot adequately mimic the conjugative effects which occur throughout these systems. Calculated chemical shifts, as can be seen below, are of little help in these efforts. The FLOCK variable evolution time sequence, developed by Bill Reynolds at the University of Toronto and scheduled to appear in the March issue of Magn. Reson. in Chem., enabled us to assign all of the carbons of Yellow No. 6 except 1 and 4a. The experiment would have permitted these resonances to be distinguished, but 2-bond C-H coupling constants are generally too small in aromatic systems to effect the necessary magnetization transfer. The structure of Yellow No. 6, carbon assignments, and calculated values, Gelbcke et al., Anal. Lett., 13, 975 (1980), are given below.

Position	Observed	n _H	Calculated
1	128.8*	0	133.4
-2	178.4	0	149.7
3	126.2	1	120.5
4	142.6	1	134.2
4a	127.0*	0	128.3
5	126.4	1	125.9
6	140.6	0	137.5
7	126.1	1	122.8
8	122.1	1	127.8
.8a	134.1	0	130.0
1'	142.8	0	155.9
2'/6'	116.7	1	123.6
3'/5'	127.3	1	126.8
4 '	140.1	0	145.8



Sincerely,

E. P. Mazzola

UNIVERSITY OF CALIFORNIA, LOS ANGELES

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Professor Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, California, 94303

SANTA BARBARA 🔸 SANTA CRUZ

DEPARTMENT OF CHEMISTRY AND BIOCHEMISTRY 405 HILGARD AVENUE LOS ANGELES, CALIFORNIA 90024-1569 January 31, 1989

High-Accuracy Integrals; Comments on Integrals

Dear Barry:

We have recently become interested in measuring integrals to as high an accuracy as possible for a particular problem, but our experience may also be of general interest. As is known, the errors in such results depend on the signal-to-noise ratio, the spectrometer stability, the line width and shape, the peak separation, the dynamic range, the avoidance of saturation and unwanted NOE's, any base-line flattening procedure used, any line broadening or sharpening procedure used, the actual integration or peak fitting procedure used (including personal biases and the unwarranted rejection of any data), and (possibly) the phase of the moon! As the required accuracy becomes greater, so does the need to avoid systematic errors and subtle artifacts.

The system that we have been studying is a very simple one, namely the ²H {¹H} spectrum of cyclohexane-d₁ at -95 °C. There are just two rather well separated lines ($\Delta v = 36.2$ Hz on a Bruker AM 500 MHz spectrometer; line width at half-height = 1.3 Hz in CS₂-5% CD₂Cl₂) of nearly the same intensities. The difference in the integrated intensities of the axial and equatorial deuteron signals gives the conformational preference (Winstein's A value) of deuterium in cyclohexane-*d*₁, and this approach to obtaining that quantity was first reported a number of years ago (R. Aydin and H. Günther, *Angew. Chem., Int. Ed. Engl.* **1981**, *20*, 985-986) on a Bruker WH 400 MHz spectrometer (at -85 °C, these workers reported an equilibrium constant of $1/K_{ea} = 1.060 \pm 0.014$, i.e., $K_{ea} = 0.9434 \pm 0.0135$, favoring the equatorial position by 22 ± 5 cal/mol). However, later work in our laboratory using Saunders' isotopic perturbation method at room temperature on cyclohexane-*d*₁₀ isotopomers gave an A value of 6.3 ± 1.5 cal/mol (F. A. L. Anet and M. Kopelevich, *J. Am. Chem. Soc.* **1986**, *108*, 1355-1356).

We have therefore tried to re-measure the A value of deuterium in cylohexane- d_1 by Günther's integration method. We have found that it is extremely easy to obtain spurious results, in large part because the lines are not extremely sharp and therefore overlap very slightly, and establishing symmetrical peaks and a flat base line is of critical importance. The alternating sampling of the real and imaginary part of the FID (which is used in Bruker spectrometers) introduces problems with obtaining a flat baseline unless a special non-standard procedure is used. This procedure, which we now describe, has been used by other workers, but does not seem to be widely known, and was brought to our attention by Dr. Mike Geckle, who also helped us to implement it. The frequency-independent and frequency-dependent phase corrections (PC0 and PC1) were set to 270 and 180° respectively. With the transmitter frequency set on resonance for a peak (CD₂Cl₂ in our case), a microprogram [1 ZE; 2 D1; 3 P1 PH1; 4 D5; 5 D5 PH0; 6 D6 ADC; 7 RCYC = 2 PH2; with PH1 = 0, 2, 1, 3 and PH2 = R0, R2, R1, R3] was used to phase that peak by adjusting the value of PH0 (360). The other peaks (i.e., those of cyclohexanc- d_1) were then phased by adjustments of the delay (D5) between the end of the pulse and the start of data acquisition and/or by slight variations in the filter band-width parameter (FW). The base line produced is very flat and requires little or no correction before peaks are integrated.

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Our integration results, obtained as the average of three independent integrations (one done blindly, where the person knew nothing about the previous history of the problem) on 8 separate sets of high signal-to-noise FID data, give $K_{ea} = 0.977 \pm 0.002$, corresponding to an A value of 8.2 ± 0.9 . The error in K_{ea} does not, of course, account for any possible remaining systematic errors, and we plan to test our integration result by integrations on *cis*- and *trans*-cylohexane-1,4-*d*₂.

We would like to hear through the Newsletter or personally of other attempts to measure integrals with an error of a small fraction of 1% (our definition of a *high-accuracy integral*). The question of integral accuracy in connection with a particular chemical problem has been investigated recently by Zvi Rappoport (see review in *Acc. Chem. Res.* **1988**, *21*, 442-449), although not at the level of accuracy needed for the cyclohexane problem. By the way, differences in intensities of the *same* peak under different conditions (as in difference spectroscopy) are much easier to obtain than the relative intensities of *different* peaks that more or less overlap.

The above work will appear in Tetrahedron Letters, and we hope to present it as a poster at the ENC in April.

.

Finally, a couple of comments on peak intensities and integrals in NMR (cf., Ray Freeman's treatment of intensities in his excellent *A Handbook of Nuclear Magnetic Resonance*):

(a) It is generally stated explicitly that quantitative NMR work requires that the area of each peak (or group of peaks) in a spectrum be *proportional to the number of nuclei* contributing to the peak(s). Whilst it is true that certain quantitative analyses, as in the work described above, demand this constraint, others do not. Quantitative work using ultraviolet, visible or infrared spectroscopy is routinely done, even though the above type of constraint is never met and each peak has its own extinction coefficient! Quantitative NMR analyses in many cases do not require that peak areas be proportional to the number of nuclei (thus, saturation or partial NOE's can be present), as for example in the analyses of mixtures of known compounds (especially in dilute solutions), where standard samples can be made for calibration purposes. The only requirement is that these saturation and NOE effects be reproducible between samples with the same spectrometer parameters. The distinction between these two types of integrals (**fixed-proportional** and **variable-proportional**) is not properly recognized in the NMR literature, and indeed, there is a lack of convenient names for these two methods. Discussions of quantitative aspects of NMR should not ignore the value of the latter type of integrals, as is generally done currently.

(b) The importance of a correct first point in the FID for obtaining accurate integrals is sometimes exaggerated. It is true, mathematically, that if the first point in the time domain is zero, then the total integral in the frequency domain is zero. However, integrals of sharp peaks over a narrow frequency range can still be reliably obtained! Also, Gaussian-Lorentzian line narrowing, which strongly affects the first part of the FID, does not necessarily invalidate peak integral information.

Please consider this letter as meeting Jane Strouse's contribution requirements.

Sincerely yours

Frank A. L. Anet and Dan J. O'Leary

Altona and Karplus type calculations on a MacIntosh

M. J. Minch and C. Ward, Departments of Chemistry and Mathematics University of the Pacific, Stockton, CA 95211

(received 2/17/89)

Vicinal proton coupling constants are a function not only of the time averaged orientation of each substituent with respect to the coupled proton pair, but also the electronegativity of all substituents bound to the H-C-C-H fragment. A number of useful general rules and semi-empirical Karplus-type equations, correcting for substituent electronegativity, have been developed from J-values for rigid ring couplings. This includes the useful equation of Altona Haasnoot, and DeLeeuw (Tetrahedron, 36 (1980) 2783-2792) which is a six-term expression based on MO theory with parameters that are functions of both the electronegativity of the first (α) and second (β) atoms of each substituent, as well as the torsion angle and orientation, with the whole expression parametrized by statistical correlation to 315 experimental coupling constants, covering a wide range of rigid compounds and substituents.

$${}^{3}J = P_{1}\cos^{2}\phi + P_{2}\cos\phi + \Sigma\Delta\chi_{i} \{P_{3} + P_{4}\cos^{2}(\zeta_{i}\cdot\phi + P_{5} \mid \Delta\chi_{i}|\}$$
(1)

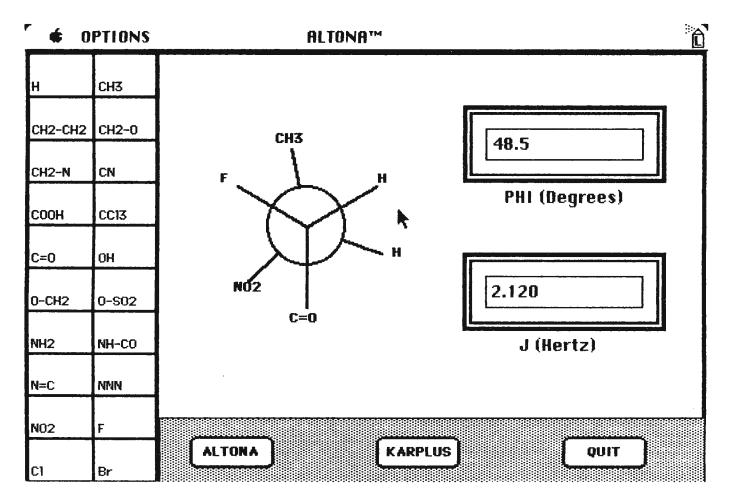
For substituents containing β-atoms

$$\Delta \chi_i = \Delta \chi^{\alpha-\text{atom}} - P_6 \Sigma \Delta \chi^{\beta_i-\text{atoms}}$$
 where $\Delta \chi_i = \chi_{\text{atom}} i^- \chi_H$

 ζ_i is ±1 depending on the substituet orientation, and $\Delta \chi_i$ is calculated from the Huggins electronegativity.

We have recently developed an easy-to-use program, ALTONA based on Equation (1) and employing interactive graphics written for the MacIntoshTM computer. The program calculates torsion angles from observed J-values or the reverse, J-values from known torsion angles, using four different versions of the Karplus equation or the Altona equation. The calculated geometry is revealed as a Newman projection down the C-C bond. The user selects the substituents about this C-C bond from a menu and types in a dihedral angle to calculate coupling constants. Plots of J vs. angle are also provided.

This program is available to interested spectroscopists with MacIntosh computers for \$10.00. Please do not send disks! Make checks out to Coburn Ward and allow three-to-four weeks for delivery of one copy of the program on a 800 K 3.5 inch disk with instructions for its use. Call for additional details (209) 946-2442.





Professor B.L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303 Department of Chemistry Fort Collins, Colorado 80523 (303) 491-6480

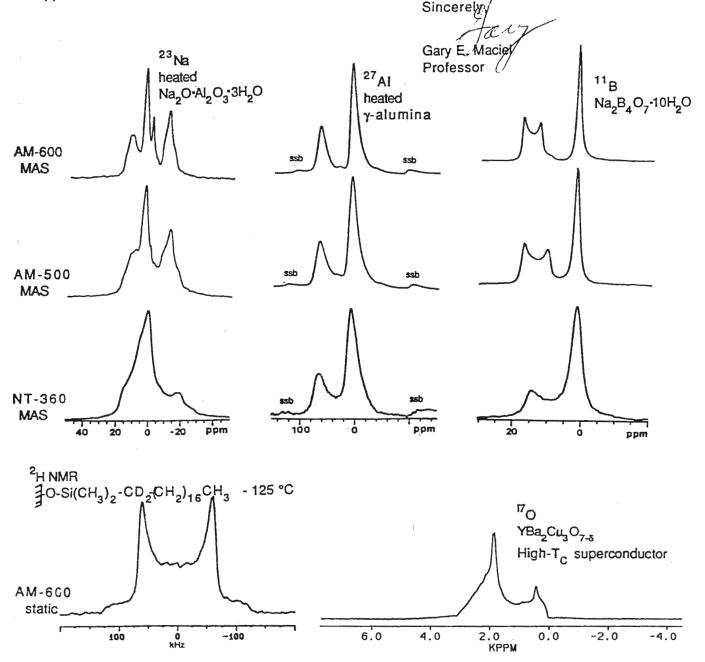
> January 26, 1989 (received 2/1/89)

Solid State NMR Results on the AM-600; Postdoctoral Position Available.

Dear Barry:

Performance of the AM-600 spectrometer, installed in the C.S.U. Regional NMR Center (303-491-6455) several months ago, has been outstanding. We have expended a considerable effort examining the field dependence of $-1/2 \leftrightarrow 1/2$ spectra of quadrupolar nuclides under conditions of high-speed MAS. Thanks to a high-speed digitizer built by Bruce Hawkins, we have also obtained excellent wide-line performance. The spectra below demonstrate the kinds of results we have been obtaining.

Beginning about July, 1989, a postdoctoral position will become available in the Center. Applicants interested in details should contact me.



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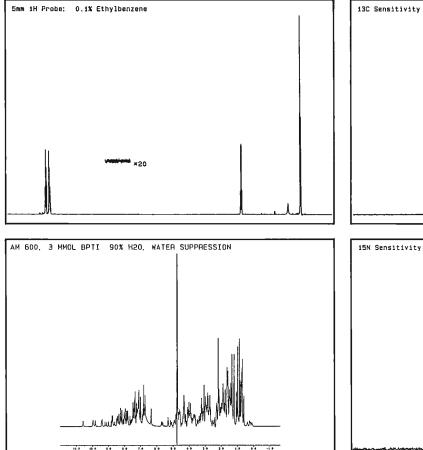
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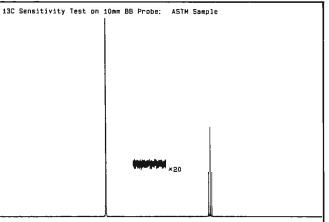
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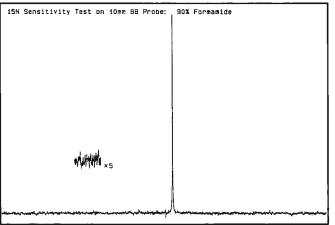
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	15N	S/N (FORM)	25:1
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	15N	S/N (FÖRM)	80:1
Resolution (all probes)			0.25 Hz





Magnet drift: ca. <40 Hz/hr

EB	 ethylbenzene with ¹H decoupling
ASTM	$= 60\% C_6 D_6$ in dioxane
FORM	 Formamide (¹H decoupling without
	NOE)
LINESHAPE:	$^{1}\text{H} = \text{CHC1}_{3}$ linewidth at height of ^{13}C
	satellite/at 20% this level
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319/356-2188 If no answer, 356-1616



February 13, 1989 (received 2/17/89)

Dr. Bernard L. Shapiro Editor, TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303

Dear Dr. Shapiro,

In clinical settings the inherent insensitivity of NMR mandates the need for optimal acquisition methods to permit decreased patient examination time. Multi-dimensional imaging and spectroscopy are most often performed with pulses sequences in which the raw data are obtained on a regular rectangular sampling grid. This pattern is inefficient for the isotropically band-limited objects commonly studied. Data points and time can be eliminated if efficient sampling patterns are used instead. I am evaluating the potential of these optimally-efficient methods in collaboration with Bill Thoma and our clinicians.

For isotropically band-limited functions in 2 dimensions, a hexagonal sampling grid is most efficient; in 3 dimensions, a body-centered cubic (BCC) grid is most efficient (see Figure 1). These optimal sampling patterns are advantageous because they require 13.4% and 29.3% fewer data points, for 2 and 3 dimensions respectively, than rectangular sampling methods. This gain can be used to either reduce the data acquisition time while maintaining image resolution or to improve the image resolution while maintaining the imaging time. For echo-planar imaging optimal sampling would lower the data rate requirements. A disadvantage of these efficient sampling techniques is that they use less data; hence, the signal-to-noise ratio of the results will be lower. For some 2-dimensional NMR spectroscopy applications this technique may not be useful because complete coverage of a rectangular frequency domain is required.

A modified DFT was derived which uses non-rectangular input points. However, the output points from this new transform are calculated on a rectangular grid because this is the pattern used by commercial hardware and software for image display and analysis. Fast algorithms for each of the efficiently-sampled multi-dimensional cases have been developed.(1,2) Without these algorithms, lengthy reconstruction times would render the efficient sampling schemes impractical.

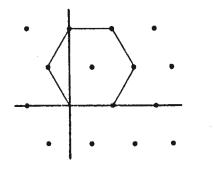
Imaging in 3-dimensions may be implemented with a frequency-encoding gradient and 2 phase-encoding (PE) gradients. Hexagonal sampling in the 2 PE dimensions is accomplished by proper choice of the PE gradient stepping pattern. Thirteen percent fewer PE steps are required. In 4-dimensional chemical shift imaging optimal sampling in the 3 spatial dimensions with a 29% efficiency gain is achieved by choosing the stepping pattern of the 3 PE gradients appropriately.

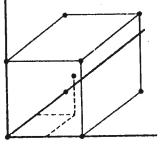
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The method assumes a band-limited source. This is equivalent to imaging a finite sized object. If the actual object is larger than the assumed size, the DFT produces aliasing. The pattern of this aliasing is given by the reciprocal lattice vectors of the sampling pattern. For rectangular sampling the aliasing occurs along the coordinate axes, but for hexagonal and BCC sampling the aliasing occurs primarily along the diagonals. This is an advantage because, in most imaging situations, the body tends to be elongated along an axis. Thus, optimal sampling may reduce aliasing problems.

References: (1) J.C. Ehrhardt, Soc. Mag. Res. Med., Book of Abstracts, 1087, 1988. (2) R.M. Mersereau and T.C. Speake, IEEE Trans. ASSP, 29,1011, 1981

Figure 1. On the left is a hexagonal grid of sampling points. On the right is a body-centered cubic grid of sampling points.



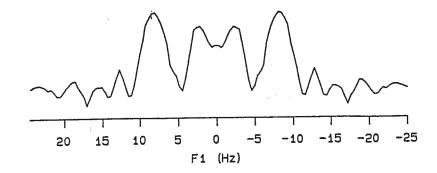


Sincerely,

James C. Ehrhardt, PhD Professor

- Continued from p. 45

The spectrum is a slice showing the $J_{\rm HH}$ of the H_1 , proton of the labeled U of the DNA duplex. The spectrum shown is for the minor form of the DNA duplex. Both forms are in the C2'-endo family and a complete report on comparing the two conformational forms is in progress.





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February 15, 1989 (received 2/21/89)

DEPARTMENT OF CHEMISTRY

B.L. Shapiro Tamu NMR Newsletter 966 Elsinore Court Palo Alto, CA 99303

Proton Detection Spectroscopy of DNA

Dear Barry:

Recently we obtained ¹³C NMR data on a sample of duplex DNA of the sequence d(CCGUGCC) paired with d(GGCACGG) in which the U was labeled in the 1' and 3' positions with ¹³C. The data showed that both the 1' and 3' sites were present in at least two environments. The ¹³C NMR results showed that both sites exhibited two signals with the ratio between the intensities of the two forms changing with temperature and the signals from the two forms coalescing when the duplex was melted (J. Am. Chem. Soc. 109, 7217). The temperature dependent behavior was found to be completely reversible.

To obtain more information about this conformational equilibrium we have begun to perform a series of proton detection experiments on the labeled DNA. The proton signals of the 1' and 3' protons also exhibit two sets of signals each. One of the more informative experiments has been the use of ¹³C filtered proton-proton J spectroscopy which allows, in principle, rather high resolution determination of the proton-proton couplings which can be related to DNA conformation. We have been using the pulse sequence

¹H: 90-tau t1/2-180-t1/2-tau-acquisition

¹³C:

90-90-

-decoupling

to obtain data such as that shown in the figure for the two 1' sites. These and other data are now being analysed to determine the conformations of the two forms of this DNA duplex and how the two conformations differ.

Sincerely.

Philip H. Bolton Associate Professor

- Continued on p. 44

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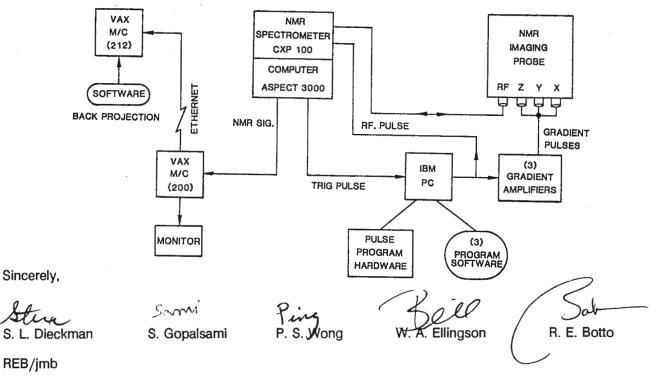
Dr. Bernard L. Shapiro Editor/Publisher TAMU NMR Newsletter 966 Elisnore Court Palo Alto, CA 94303

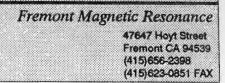
RE: Imaging of Solids on CXP-100 Spectrometer

Dear Barry:

We have become increasingly interested in the NMR imaging of short T_2 polymeric materials as applied to aspects of materials research. Our present application involves the determination of the distribution of multicomponent polymeric additives in advanced green ceramic components [Development of Nuclear Magnetic Resonance Imaging Technology for Advanced Ceramics, Argonne National Laborjatory Report ANL-87-53 (November, 1988).] Because of the short proton T_2 s (typically less than 0.5 msec) of these materials, large magnetic field gradients are required to obtain the desired spatial resolution in the image. Additionally, the length of the T_2 also makes filtered back projection imaging techniques the method of choice over more widely used recalled echo techniques. To facilitate these experiments, we have designed and have begun to test a home-built imaging accessory for our Bruker CXP-100 spectrometer.

A block diagram of the imaging system is presented in the figure below. The probe has been designed to provide 54 g/cm and a 28 mm working sample diameter. An IBM PC based pulse programmer will provide RF pulse shaping and magnetic field gradient control. Experimental data will be acquired on the Bruker spectrometer and will then be ported from the Aspect 3000 to Argonne's VAX 8700 via ethernet for image reconstruction and processing.





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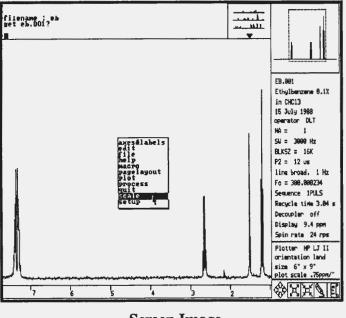
We offer an RF module and probe repair services. Modules and probes can be expressed to our facilities for repair by our trained technicians at reasonable rates. Repaired items can be returned air express for minimum down-time. Call us for time and price estimates. Detailed quotes can be provided after inspection and before repair if desired.

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PLOT is a software tool requiring an IBM PC or compatible, and supports common graphics devices, mice, plotters and printers. The transformed data file is transferred to the PC by RS-232, Kermit, Ethernet, or by emulating the spectrometer's plotter. PLOT is WYSIWYG, which means you can preview your plot on the computer screen as it will appear on paper. Recently accessed spectra are kept in a stack similar to an HP calculator for easy manipulating and viewing.

PLOT will work with CGA, EGA, VGA, Hercules, AT&T, or Tandy graphics systems. It will employ a 8087 coprocessor if it finds one. It can output your data to an HP-compatible laser printer, an HPGL plotter, A Zeta plotter, an Epson-compatible dot matrix printer, to a file in any of the above formats, or to a file for input into Aldus PageMaker or Xerox Ventura Publisher.

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AT&T Bell Laboratories

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February 16, 1989 (received 2/20/89)

Dr. Barry Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303

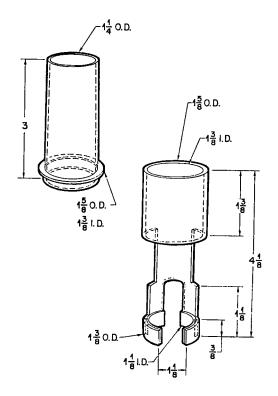
Rodent Holder and Non-invasive Modification of a Bruker NMR Microscope Probe

Dear Barry:

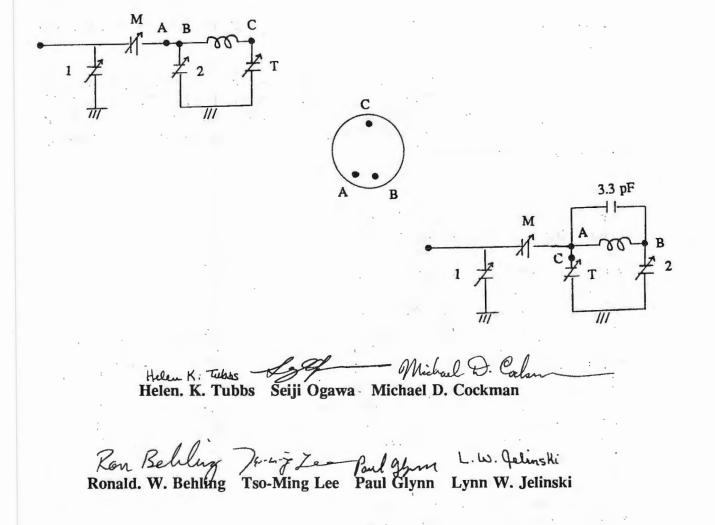
As you know, two of the most important requirements for microimaging on animals are (1) a highly reliable system for positioning and restraining the animal, and (2) excellent signal-to-noise. We have developed two modifications for the Bruker NMR Microscope probe that are invaluable for obtaining high resolution, high sensitivity surface coil images of rodents.

We show here a rodent holder that can comfortably accommodate an 80 gram rat. The dimensions are in inches. The significant aspects of this design are (i) it attaches firmly to the probe body, using the same screws and holes that were originally used to hold the volume imaging coil in place; (ii) it provides reliable and reproducible positioning; (iii) the tapered top allows easy insertion into the bore of the magnet; and (iv) breathing artifacts are minimized because the rodent can be gently taped into place.

The holder is made of clear acrylic tubing, available from Acme Plastics of Patterson, New Jersey. Chloroform or Craftics #33 clear thickened cement can be used to glue the parts together. The top is tapered and milled out on the inside.



The other modification concerns a plug-compatible surface coil. The original circuit for the 20 mm volume imaging coil (left) can be modified "non-invasively" by removing the volume imaging coil from its plug-in socket (center, top-down view of socket). A teflon coated copper surface coil is fabricated (1 turn, 1 cm diameter) that has a 3.3 pF capacitor soldered across leads A and B. The coil, with legs A and C connected together, is placed in the circuit (right). The capacitor connecting A and B removes the "legs" from the circuit and greatly reduces the inductance of the coil, making the coil "loop" the only source of radio emission and detection. In these diagrams, 1, 2, M (match), and T (tune) are the original capacitors in the circuit for the original 20 mm coil. The inductor in the left diagram is the volume imaging coil; the inductor in the right diagram is the surface imaging coil.





McMASTER UNIVERSITY Department of Chemistry 1280 Main Street West, Hamilton, Ontario L8S 4M1 Telephone: (416) 525-9140 FAXMAIL (416) 528-5030

> February 2nd, 1989 (received 2/11/89)

Dr. B. L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA. 94303 U.S.A.

DEUTERATED SOLVENT FOR HIGH TEMPERATURE POLYMER NMR

Dear Barry:

Carbon-13 NMR is commonly used to determine branching in polymers particularly in polyethylene and polypropylene. These spectra are usually obtained as 15% solutions in 1,2,4 trichlorobenzene at 120-140C. Long term resolution stability becomes difficult at this temperature and hence it was decided to deuterate the solvent. The FID shown in figure 1 was the result of 16 hours accumulation and the resulting spectrum in figure 2 indicates the resolution that can be obtained.

A limited amount of this solvent is available; contact NHW for further information and costs.

B.G. Sayer

٦

G. Timmins N.H. Werstiuk

Please credit this contribution to the account of A.D. Bain.

Fig.1. FID of polypropylene in 1,2,4 trichlorobenzene after 16 hours

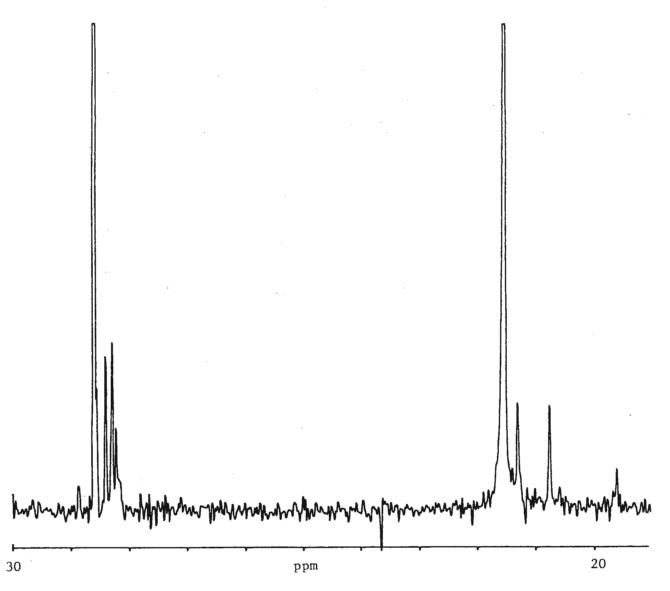


Fig.2. Part of carbon-13 NMR spectrum of polypropylene

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Dear Dr. Shapiro,

The graduate students of the University of Rhode Island's Chemistry Dept. present their 11th Symposium entitled, "NMR STATE OF THE ART AND FUTURE DIRECTIONS" on April 29, 1989.

Dr. Joseph J.H. Ackerman (Washington Univ.) will speak on the topic of, Invivo NMR Spectroscopy, Dr. Ad Bax (NIH) will discuss recent developments in, Two- and Three- Dimensional NMR. Dr. Gary E. Maciel (Colorado State Univ.) will talk about "High Resolution ¹H NMR of Solids". Dr. Alexander Pines (UC Berkeley and National Academy of Sciences) entitles his lecture "There's No Free Induction" and Dr. Jacob C.A. Schaefer (Washington Univ.) will discuss the detection of weak ${}^{13}C_{-}{}^{15}N$ dipolar coupling by "Magic-Angle Spinning NMR".

We extend an invitation to all graduate students working in the field of NMR to present their research at our Poster Session during the symposium.

Registration is requested and the charge is \$18.00 per person (nonstudent). For more information please contact Brad Sherman or Robyn Pothier, (401) 792-2203 Dept. of Chemistry, University of Rhode Island, Kingston, RI 02881.

The Graduate Student Symposium Committee would greatly appreciate your listing of our symposium in the March or April issue.

Thankyou for your time, Robyn. Pothier

Robyn Pothier co-chairperson



DOW CHEMICAL U.S.A.

February 10, 1989 (received 2/17/89)

TEXAS OPERATIONS FREEPORT, TEXAS 77541

Dr. Barry L. Shapiro Editor/Publisher TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303

Dear Dr. Shapiro,

Although automatic sample changers are available for most commercial NMR spectrometers, not all manufacturers allow for the changing of samples which are at temperatures other than ambient. The need for maintaining samples at an elevated temperature prior to introduction into the superconducting magnet is particularly important when, as in our laboratory, numerous polyolefin copolymers must be analyzed. These samples need to be kept at 130 degrees C both before and during analysis by carbon-13 NMR. We describe here a system which utilizes a Zymark robot to automatically load, run and unload up to nine samples on a JEOL GX-400 NMR. Our goal was to attach the robot to the NMR in such a manner that samples could be picked up from a hot block, placed in the NMR and then retrieved after the run was complete. Also, we did not wish to become involved in modification of the basic vendor supplied NMR programs or hardware.

The layout of our system is shown in Figure 1. In operation, NMR tubes which are already fitted with spinners are placed in an insulated metal block which is heated by a standard laboratory hot plate (Thermolyne type 2200) and equipped with an over-temperature cutoff. The basic sequence of movements by the robot is triggered by the ejection of a sample. The detection of an eject signal by the power and event controller of the robot uses the only spectrometer hardware modification necessary for the system. On the JEOL GX-400 this signal was easily obtained from the spin and sense amplifier (connector SRIN). Upon detection of an eject signal the robot retrieves the sample, confirms the sample's presence in the hand, and places it in the receiving rack. The new sample is removed from the hot block, confirmed and placed on the air cushion at the top of the superconducting magnet. During this process the macro programs of the spectrometer are in a pause mode. The robot then types a continue command on the keyboard accessible to it. Control of the instrument is restored to the spectrometers, which then proceeds to lower the sample, set up the parameters, perform necessary "touch up" shimming and begin the data acquisition. A Tektronix 4107 terminal is the normal second terminal on the JEOL system and this keyboard is used by the robot to pass control back to the spectrometer. When the robot is used, the spectrometer is thus run from the Tektronix rather than the "main" spectrometer terminal. The keyboard must be used with the autorepeat feature off and symbols such as @ must be redefined so that only a single keystroke is needed. Throughout the system, standard vendor supplied programs (such as autoshim routines) were incorporated without modification into the macro programs.



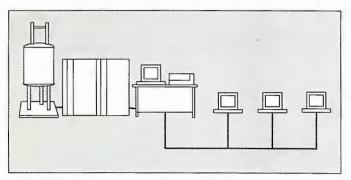




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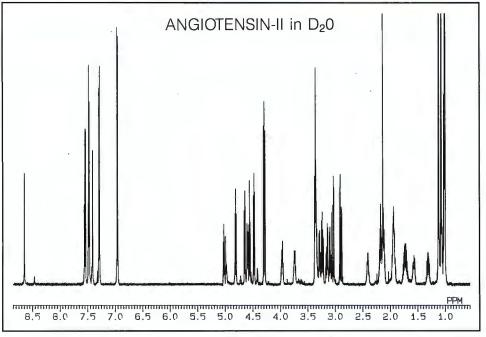
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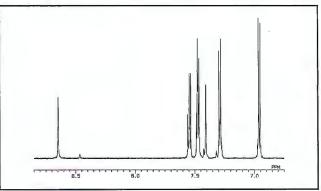
GSX-600

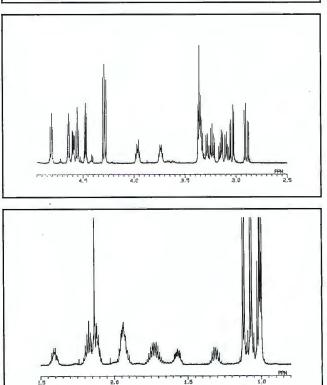


JEOL in its continuing commitment to the scientific community announces an operational 600 MHz NMR spectrometer at its Akashima applications laboratory. The Oxford Instruments 14.1 Tesla superconducting solenoid with JEOL's well proven matrix shim system, benchmark Rf technology, and excellence in probe design combine to provide the highest dispersion in 600 MHz performance. If your research and applications in macro molecules or low gamma nuclei requires 600 MHz performance, you owe it to yourself to call JEOL.

The above data is of Angiotensin-II in D_2O and was processed under normal one dimensional conditions. If you are presently evaluating 600 MHZ NMR spectrometers, we would be pleased to arrange for you to see the GSX-600.







The design of the hand is of importance, since the retrieval of an ejected sample involves the grasping of a moving target as the sample bobs on the air cushion that ejects it. This bobbing motion is greatly reduced by the plastic "cover" shown in Figure 2. The hand is lowered over the sample with the jaws at maximum separation; at the appropriate height the top of the NMR tube bobs against the plastic cover stabilizing the tube's motion. The jaws then close to grasp the sample. Confirming the presence of the sample in the hand is done by having the robot place the sample so as to interrupt the light source to a photodiode. This simple device consists of a photodiode and a light bulb mounted six inches apart and 6.5 inches high. Both the bulb and photodiode are under the control of the Zymark power and event controller.

In order to minimize the effects of the system on magnet homogeneity, the steel skirt of the robot was replaced with one made of aluminum. Also, a steel plate at the base of the Tektronix keyboard was removed and replaced with plexiglas. The table for the system consists of a plywood base with aluminum legs.

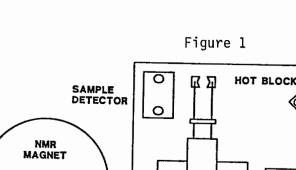
Although some steel portions of the Zymark robot could not be easily replaced, we have not experienced any significant degradation of magnet homogeneity. Small changes in the field were easily shimmed out. The homogeneity effects are minimized by locating the robot and associated hardware at the maximum possible distance (both horizontally and vertically) from the magnet. Also, the robot arm is programmed to return to a position which causes the least effect on the field and to remain there during the run. Our robot spectroscopist system is used quite frequently, and has proven to be reliable and convenient.

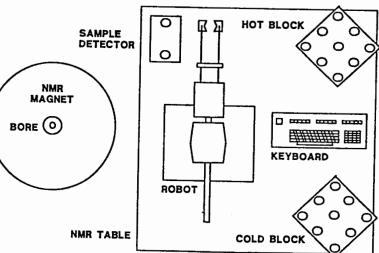
M. D. Meadows

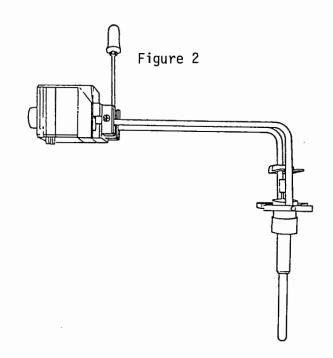
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DEPARTMENT OF CHEMISTRY

SANTA CRUZ, CALIFORNIA 95064

February 15, 1989 (received 2/17/89)

Professor Barry Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303

FREQUENCY RANGE SENSITIVITY ON GE PROBES

Dear Barry:

The high dielectric constant associated with samples of high ionic strength in aqueous solutions can alter the resonant characteristics of a probe coil beyond the capabilities of the tuning capacitors for a given frequency. We encountered this problem recently (1.2 grams of KCL in D_2O) on our dedicated GE (GN-300) Widebore 12mm Potassium Probe (14.MHz).

Applying the concept that in a resonant circuit, the order of circuit elements in series is irrelevant [Alderman & Grant, JMR 36, 447-451 (1979)] we have been successful in increasing the frequency range of our Potassium probe as well as "Broadbanding" a dedicated 5mm C/H probe to tune from 70 MHz (59 CO) through 121 MHz (31 P) with no observable decrease in signal to noise and line shape. At 5mm the Proton 90° pulse at approximately 75 watts (60db) remained 13 usec; 90° pulse for 13 C is 12 usec (ASTM) and for Ammonium Phosphate in D20 the 31 P 90° pulse is 10 usec after the modification.

Although the circuitry is well known to all, [Murphy-Boesch, Biomedical Magnetic Resonance (1984)] we used the same basic LC configuration on both probes. Figure 1. is the Carbon-13 circuit modification and Figure 2. the Potassium-39 modification. All the variable capacitors are tunable to 12 pf. The fixed porcelain capacitor was empirically selected. The "shorting" stick (Figure 1) is disengaged for frequencies between 79 MHz (²³Na) and 121 MHz.



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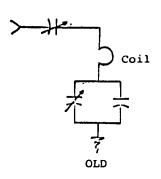
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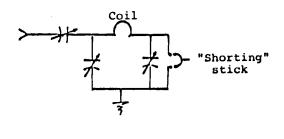
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Figure 1. Carbon-13 Probe Coil

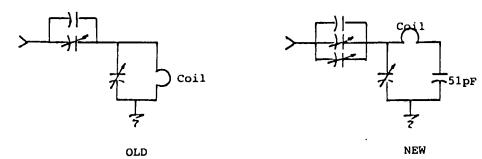


Figure 2. Potassium-39 Probe Coil

Sincerely Jim Loo



Professor B L Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto California CA 94303 USA

Wilton Materials Research Centre

ICI Advanced Materials ICI Films ICI Chemicals & Polymers Ltd

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Direct line	Tel Ext	Date
	6413	23 January 1989
		(received 1/28/89)

Dear Barry

Your ref.

VARIABLE TEMPERATURE IMAGING

Our ref

S1PJ201M\LE

We have been using a Bruker MSL-200 spectrometer, equipped with mini-imaging accessories, to investigate applications of MRI in materials science. Many of our samples have T_2S that are too short to allow signals to be generated by standard biomedical Fourier techniques. Our modified probe and improved gradient performance now enables echo times of the order of 2 ms to be used. Even so, T_2S from rigid solids, cross-linked polymers and strongly bound absorbed solvents may still be too short for observation. T_2S may be extended by operating at elevated temperatures by increasing the degree of molecular or chain-segment motion present in solids. In particular, polymers observed above the Tg can give liquid-like signals.

We have constructed a variable-temperature imaging probe consisting of a horizontally mounted solenoid, wound from 3 mm copper ribbon (3 cm x 1.5 cm) surrounded by a standard Bruker wide-line probe dewar and fitted with a thermocouple, supply gas dewar and heater. The probe can operate at temperatures between -120°C and +100°C, though, as yet, only high temperature operation has been investigated thoroughly. The low-Q r.f. circuit also allows multiple-pulse (MREV-8, etc) line-narrowing sequences to be performed, enabling solid materials to be imaged directly. The coil has good r.f. homogeneity over a volume approximately 1.2 cm by 2.0 cm, enabling small-scale materials to be imaged. With gradients up to 12 G/cm, resolution of ca 100 microns can be routinely achieved on typical samples.

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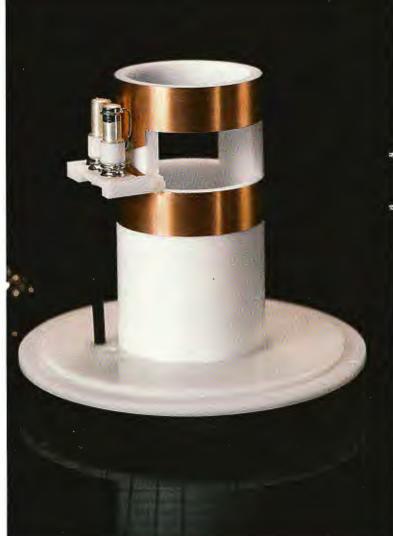
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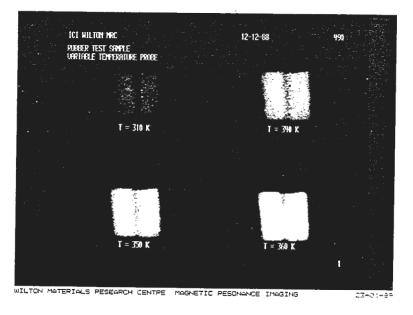
The figure shows images generated from a sample comprised of two blocks of a crosslinked rubber separated by a sheet of paper, obtained at 310, 340, 350 and 360K. The 128 x 128 images were obtained with single-transient acquisition, requiring only 64 seconds to complete. A hard 90 - hard 180 sequence was used, with an echo time of 2.2 ms. At room temperature, no signal is observed without extensive signal averaging. The benefits from high temperature imaging of such samples are apparent.

- 2 -

Can you please credit this contribution to A Bunn's account.

Yours sincerely

PETE JACKSON



I can't abide empty space, and there is nothing on hand which is the right size for this 'hole', so herewith a *tout* for a wee book related only indirectly to the pursuit of salvation through NMR spectroscopy. The subtitle notwithstanding, it will, I am sure, be found both entertaining and useful by those who toil outside of Academe as well as those within.

"Microcosmographia Academica - Being a guide for the young academic politician" - by F. M. Cornford.

Bowes & Bowes (Publishers) Ltd., 9 Bow Street, Covent Garden, London WC2E 7AL, England. ISBN 0 370 00145 1. First published in 1908, and reprinted numerous times, including in a very inexpensive paper-back edition in 1983 (and perhaps even more recently). The price at the Bowes & Bowes shop in Cambridge in 1983 was £1.95.

B.L.S.



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CENTRAL RESEARCH & DEVELOPMENT DEPARTMENT EXPERIMENTAL STATION

February 13, 1989

Dr. Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303

Copper Spin Counting in High T_c Superconductors

Dear Barry:

Our experience with solid-state NMR applications in zeolites has made us aware of the great importance of spin counting in inhomogeneous and nonstoichiometric systems. Thus, when we began Cu NQR and NMR measurements on the high- T_c superconductor $YBa_2Cu_3O_x$ (6<x<7) a little over a year ago, we first wanted to find out whether we were seeing 1%, 10% or 100% of all the coppers in the sample and whether relative signal intensities were quantitatively reliable. This letter summarizes some of what we did to answer these questions.

The Cu NQR spectra consist of 1 to 5 MHz wide peaks that cover the frequency range from 20 to 31 MHz. They must be obtained point-by-point with a spin echo method. All measurements are done with a CXP300 at room temperature. We use pulses of 4 and 8 µs, giving rise to echoes that represents 0.3 MHz-wide slices out of the broad spectral distribution. Since the FT of the echoes have a universal shape that is entirely determined by the pulse amplitude and widths, measuring the echo amplitude by visual curve fitting to a standard signal is simple and straightforward. Doing this in frequency space has the added advantage that spurious signals from external transmissions (of which Wilmington has plenty around 30 MHz) are usually well distinguishable from the spin echo signal.

The real difficulty is the calibration of signal intensities over a wide frequency range. If we start with the simplifying assumption that at the top of the echo all the resonant spins point along the "x direction", then the detected signal amplitude, S, at resonance frequency, v, is related to the number of spins, N, through the relation (Abragam, page 72) S=N γ I(I+1) v^2 f(v), where f(v) stands for the combined response function of the rf coil, probe, transmission line, amplifier, and detector. In this form, the equation allows comparison between signals of nuclei with any γ and at any resonance frequency. Since f(v) is the only uncertain factor in the equation, a full characterization of its behavior completes the quantitative evaluation of our detection method. In the hope that f(v) could be made frequency independent, we constructed a probe insert that is tunable from 18 to 40 MHz. However, above and below 30 MHz we have to use different power-amplifier inserts and preamplifier matching boxes, while for each frequency point in the spectrum we must tune the probe, the power amplifier, and preamplifier. The following quantitative signal comparisons were made to test f(v).

1. NMR in 7.05 T of an aqueous solution of NH_4Cl at the three resonance frequencies of ${}^{35}Cl$, ${}^{37}Cl$, and ${}^{14}N$. At each frequency the FID amplitude was measured following an optimized 90° pulse. The numbers of spins were proportional to the natural abundances. The normalized results were:

Hare Research, Inc. 14810 216th NE Woodinville WA 98072 Tel: (206) 789-7559 FAX: (206) 788-2552

Barry -

Subject: Automated NOE Identification

To determine the three-dimensional structure of a biopolymer, one must first perform the tedious task of assigning the resonances in the spectrum. Following that a second timeconsuming and potentially tricky process is the identification of the hundreds to thousands of NOEs in a NOESY spectrum. This step entails not only identifying as many NOE cross peaks as possible, but also determining a distance estimate (or distance range estimate) from the NOE buildup rate. This information is stored for use in calculating the molecule's structure.

During this long and tedious process it is quite possible that one misidentifies an NOE given human nature, or perhaps by forgetting the possibility that the peak could arise from a proton that was not assigned (few large molecules are completely assigned). A second error that has happened to several researchers is identifying the NOE correctly, but writing it (or the distance range) incorrectly in the input file for the structure determination program.

These problems are avoided and the process greatly facilitated if an automated NOE identification routine is used. This routine involves comparing an assignment list to a NOESY cross peak list—a simple process, though now performed much faster without the chance of transcriptional errors. Distance ranges are automatically determined (either strong/medium/weak ranges, or determined from a scaled distance estimate) and the output can be read directly by the structure calculation program (in this case **D**SPACE).

This is only possible, of course, when the identity of the NOE is unambiguous. When several possible identities exist for a given NOE cross peak it is useful to utilize available distance information such as an average structure obtained from several structures where the standard deviation in atomic position is also calculated. This information is used to check interatomic distances for all possible parent pairs for ambiguous NOE cross peaks. For example, a peak in a protein spectrum occurs at 8.54 ppm, 2.89 ppm); there are three amide protons assigned at 8.54 ppm and two protons assigned at 2.89 ppm, giving rise to six different pairs of parents. A check of the average structure however shows only one possible pair within 4Å (including a standard deviation or two). This peak is now identified!

But maybe not, if there is an unassigned amide proton within 4Å of either proton at 2.89 ppm. Thus feature of an automated NOE identification program should be to check for the presense of unassigned protons. In this case it is useful to write the "identified" NOE and distance range, but comment that line out. What happens now is up to the user. Maybe he or she will use this information to get some more resonance assignments, an easier process with the tools provided by intelligent automation programs.

Aur -Paul L. Weber

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- •Built-in NOESY backcalculation from structure data.
- •Automatic NOESY cross peak identification (maybe).

We will also be glad to show you our software for NMR-based structure determination (DSPACE).

Play with our computers, have a beer, tell us what you like and don't like about our software, have another beer, or just hang out and talk science with Paul and Dennis.

See you in April!



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Nucleus	Frequency	$S/(N\gamma I(I+1)v^2)$
³⁵ Cl	29.4 MHz	0.96
³⁷ Cl	24.5 MHz	1.04
¹⁴ N	21.7 MHz	0.34

2. 35 Cl NQR in zero field of weighed samples of K₂PtCl₆ and K₂IrCl₆. These Cl compounds were identified after an extensive search in Ref. [1] and an intensive consultation with du Pont colleagues concerning the availability, safety, and purity of prospective samples. The signal amplitudes were determined from extrapolation of echo intensities to τ =0 in a two-pulse sequence. Normalized results:

Sample	Frequency	T ₂	$S/(Nv^2)$
K ₂ PtCl ₆	25.81 MHz	1.3 ms (Gaussian)	1.13
K ₂ IrCl ₆	20.73 MHz	150 µs (expon'l)	0.88

3. NQR in zero field of 63 Cu a	and ⁶⁵ Cu in Cu ₂ O. N	ormalized results	5:	-
Nucleus	Frequency	Ν	γ	$S/(N\gamma^2)$
⁶³ Cu	26.0 MHz	69.1%	11.28 MHz/T	0.93
⁶⁵ Cu	24.0 MHz	30.9%	12.09 MHz/T	1.07

4. All measurements of Cu NQR intensities at 30 MHz were routinely double checked with tuning inserts for >30MHz and for <30MHz. The data always agreed within 5%.

The agreement is not perfect, but with the exception of the puzzling 14 N result, we found that all intensity measurements indicate that f(v) is a constant, within ±15%.

The remaining question is that of uniform excitation by the echo sequence. There are theoretical worries related to the orientation depencence of NQR pulse flip angles and the resulting small differences that arise in the powder summations for different asymmetry parameters. On the other hand, we found empirically that the rf power could be varied over quite a wide range without producing an appreciable change in NQR echo amplitudes. Moreover, rf power adjustment for maximum echo intensities at different Cu NQR frequencies consistently ended up at the same transmitter-gain setting. This gave us confidence that there are no serious problems with the excitation aspect of the NQR spin counting. More or less encouraged by this evaluation, we finally dared to draw some cautious quantitative conclusions from our NQR results of '123'.

Please credit this to Dr. Don Bly's account.

Sincerely

Alexander J. Vega

 G. K. Semin, T. A. Babushkina, and G. G. Yakobson, "Nuclear Quadrupole Resonance in Chemistry", transl. from Russian by A. Barouch, Keter, Jerusalem, 1975.

For Sale

A Varian XL-200 with a V-77 Data System Purchased new in 1983 Includes Console, Hard Disk Drive, and Dewar 5mm ¹³C/¹H switchable probe and 10 mm ¹³C/H probe Make us an offer we cannot refuse Michael J. Minch Department of Chemistry UOP Stockton CA 95211 (209)946-2442

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TAMU NMR Newsletter

Policies and Practical Considerations

(Revised February 1989)

The TAMU NMR Newsletter (formerly the IIT NMR Newsletter, and originally the Mellon Institute NMR Newsletter) continues with the same name, under the aegis of Texas A&M University, although the undersigned Editor/Publisher now resides in California. The Newsletter, now in its thirty-first year of consecutive monthly publication, continues under the same general policies as in the past. All communication with the Newsletter must be directed to the address overleaf.

1. Policy:

The TAMU NMR Newsletter is a means for the rapid exchange of information among active workers in the field of NMR spectroscopy, as defined broadly, including imaging. As such, the Newsletter will serve its purpose best if the participants impart whatever they feel will be of interest to their colleagues, and inquire about whatever matters concern them.

Since the subscriber/participant clearly is the best judge of what he or she considers interesting, our first statement of policy is "We print anything." (This usually is followed by the mental reservation, "that won't land us in jail.") Virtually no editorial functions are performed, although on rare occasions there is the need to classify a contribution as 'not for credit'. I trust that the reasons for this policy are obvious.

The TAMU NMR Newsletter is not, and will not become, a journal. We merely reproduce and disseminate exactly what is sent in. Foreign participants should not feel obliged to render their contributions in English.

2. Public Quotation and Referencing:

Public quotation of Newsletter contents in print or in a formal talk at a meeting, etc., is expressly forbidden (except as follows), and reference to the TAMU NMR Newsletter by name in the scientific literature is never permissible. In order to quote results or use material from the Newsletter, it is necessary, in each individual case, to obtain the prior permission of the author in question and then to refer to the material quoted as a "Private Communication". If your copy of the Newsletter is shared with other readers, it is your obligation as the actual recipient of the Newsletter to see that these other readers of your copy are acquainted with, and abide by, these statements of policy.

3. <u>Participation is the prime requisite for receiving the TAMU NMR Newsletter:</u> In order to receive the Newsletter, you must make at least occasional technical contributions to its contents.

We feel that we have to be quite rigorous in this regard, and the following schedule is in effect: Eight months after your last technical contribution you will receive a "Reminder" notice. If no technical contribution is then forthcoming, ten months after your previous contribution you will receive an "Ultimatum" notice, and then the next issue will be your last, absent a technical contribution. Subscription fees are not refunded in such cases. If you are dropped from the mailing list, you can be reinstated by submitting a contribution, and you will receive back issues (as available) and forthcoming issues at the rate of nine per contribution.

Frequent contributions are encouraged, but no "advance credit" can be obtained for them. In cases of joint authorship, either contributor, but not both, may be credited. Please indicate to whose account credit should be given. Please note that meeting announcements, as well as "Position Available," "Equipment Wanted" (or "For Sale"), etc., notices are very welcome, but only on a not-for-credit basis, *i.e.*, such items do not substitute for a *bona fide* technical contribution. Similar considerations must occasionally be applied to a few (quasi-)technical items.

4. Finances:

The Newsletter is wholly self-supporting, and depends for its funds on advertising, donations, and individual subscriptions.

The <u>Subscription</u> fee is currently US\$120.00 per year, with a 50% academic or personal discount. Subscriptions are available only for the twelve monthly issues which begin with the October issue and run through that of the following September. However, a subscription can be initiated at any time, and the issues back to the previous October will be provided as long as copies remain available.

Companies and other organizations are also invited to consider joining the list of <u>Sponsors</u> of the Newsletter. Sponsors' names appear in each month's Newsletter, and copies of the Newsletter are provided to all Sponsors. The continuation of

this non-commerical Newsletter depends significantly on the interest and generosity of our Sponsors, most of whom have been loyal supporters of this publication for many years. We will be happy to provide further details to anyone interested.

Another major, indeed most essential, source of funds for the Newsletter is <u>Advertising</u>. We earnestly encourage present and potential participants of the Newsletter to seek advertising from their companies. Our rates are very modest - please inquire for details.

5. Practical Considerations:

a) All technical contributions to the TAMU NMR Newsletter will always be included in the next issue if received before the published deadline dates.

b) Please provide short titles of all topics of your contributions, so as to ensure accuracy in the table of contents.

c) Contributions should be on the *minimum* (NOTE!!) number of $8.5 \times 11^{\circ}$ (21 x 27.5 cm) pages, printed on one side only. Contributions may not exceed three pages without prior approval. Each page must have margins of at least $0.5 - 0.75^{\circ}$ (1.3 - 2.0 cm) on all sides. Please observe these limits. Black ink for typing, drawings, etc., is essential. All drawings, figures, etc., should be mounted in place on the $8.5 \times 11^{\circ}$ pages. We are not equipped to handle pieces of paper larger than $8.5 \times 11^{\circ}$ (21 x 27.5 cm).

Foreign subscribers are reminded that regardless of the standard paper length you use, all material - letterhead, text, figures, addresses printed at the page bottom, everything - must not exceed 10" (ca. 25.3 cm) from top to bottom.

Significant savings of Newsletter pages and total space can be made by exercising close control over the formatting and type sizes of the contributions. Please consider the following:

i) For those with computers, try using a smaller type font. The body of this page is printed in 10 point type, which I believe is adequate for most purposes. Even 12 point is acceptable, I suppose. Those who are computerized can also employ non-integral spacing of lines so that sub- and superscripts don't collide with lines below and above.

ii) PLEASE avoid excessive margins. Instruct your secretaries to avoid normal correspondence esthetics or practices, however time-honored or 'standard'! This page has margins on both sides of 0.6" (ca. 1.55 cm), which is very adequate. Margins of the same size at the top and bottom are sufficient also, but don't worry if there is more space at the end of your document, for I can often use such spaces for notices, etc.

Also, please avoid large amounts of unused space at the top of letters. Give thought to the sizes of figures, drawings, etc., and please mount these so as to use the minimum space on the page.

iii) <u>'Position Available', 'Equipment Wanted', and Similar Notices</u>. These are always welcome, without charge, but not for subscription credit, of course. Such notices will appear, however, *only* if received with these necessarily rigid constraints: a) <u>Single spaced</u>; b) both side margins 0.6 - 0.7" (1.5 - 1.7 cm.)- NOT WIDER; c) the minimum total height, please, but definitely no more than 4.5" (11.5 cm.) This will let me place such notices wherever a bit of space occurs.

iv) AVOID DOUBLE SPACING LIKE THE BLACK PLAGUE !!! This is extremely wasteful of space. Even sans computer, small type and 1.5-line (if needed) spacing can be had with a little effort.

6. Suggestions: They are always welcome.

B. L. Shapiro

Address for all correspondence:

Dr. Bernard L. Shapiro Editor/Publisher TAMU NMR Newsletter 966 Elsinore Court Palo Alto, California 94303 U.S.A.

Telephone: (415) 493-5971.

TAMU NMR Newsletter

All Newsletter Correspondence Should Be Addressed To:

Dr. Bernard L. Shapiro TAMU NMR Newsletter 966 Elsinore Court Palo Alto, CA 94303, U.S.A.

(415) 493-5971

DEADLINE DATES			
No. 368 (May)21 April 1989			
No. 369 (June) 19 May 1989			
No. 370 (July) 16 June 1989			
No. 371 (August) 21 July 1989			

To those who have been so helpful in conserving space by the careful formatting of their technical contributions, using small type fonts, avoiding the sin of double-spacing lines, etc., many thanks. To those who have yet to help me save pages (*i.e.*, expense), please join the ranks of the righteous.

Again I ask that 'Position Available', 'Equipment Wanted', and similar notices be constructed so as to use the <u>minimum</u> <u>vertical space</u>. Avoiding large margins helps greatly: 1/2 - 3/4" on each side is quite sufficient. DO NOT DOUBLE SPACE THESE NOTICES!! - in future I'll send badly done notices back for re-working. I am most happy to have such notices appear in the Newsletter, without charge, for Subcribers, Sponsors, Advertisers, or indeed anyone else, but your cooperation in utilizing space efficiently will truly be appreciated.

It is heartening to note the increase in the number of Advertising pages in recent issues of the Newsletter. Some of this increase is connected with the imminent occurence of the ENC, but a more general development of the advertising component is clear. This is of obvious benefit in keeping the Subscription fee down to a tolerable level. Please assist in this process by making sure that our loyal Advertisers know that you have seen their ads in the Newsletter and appreciate their support. Despite the increased amount of advertising, still more is needed, as are additional **Sponsors**. Please do what you can to help

Let me again acknowledge with thanks the clever and artistic efforts of Wendy Goldberg and Uwe Oehler for their stodgereducing contributions to the Newsletter pages. My inventory of these NMR-related cartoons is getting very low, but I still hope that others will also step forward to provide some pictorial rays of sunshine and mirth.

B.L.S.



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TEXAS A&M UNIVERSITY

No. 366 **March 1989**



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CSI 2T Applications

Analytical techniques: localized spectroscopy

Nuclear magnetic resonance (NMR) imaging has proven to be a valuable analytical technique. But the possibility of combining imaging with NMR spectroscopy has always been a desired goal. Recently developed localization techniques now make it possible to collect NMR spectra from a region of interest determined by an NMR image.¹⁻⁵

Seven vials, each containing a different material, were imaged (Fig. 1). Using the stimulated echo technique,⁵ 5 mm cubes (125 ul) were selected, and proton NMR spectra were collected. Although this method may limit the type of RF pulse sequence used, many experiments can be performed within a specific volume, including solvent suppression (Spectrum d) and relaxation measurements (Spectrum a). Such techniques may have applications for nondestructive testing and analysis of materials.

References:

¹Bottomley, PA; Foster, TB; Darrow, RD: J. Magn. Reson., 1984, 59:338.

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⁵Frahm, J; Merboldt, KD; Hanicke, W. Works in Progress, 5th annual meeting of the Society of Magnetic Resonance in Medicine. Montreal, August, 1986, p. 158.

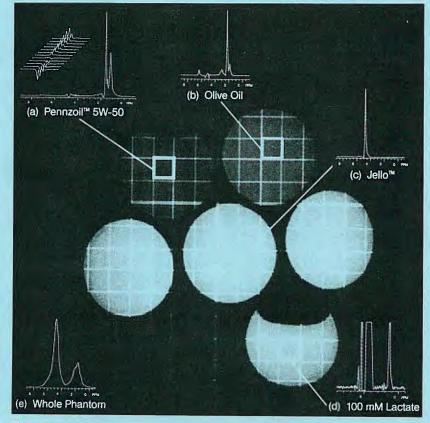


Fig. 1



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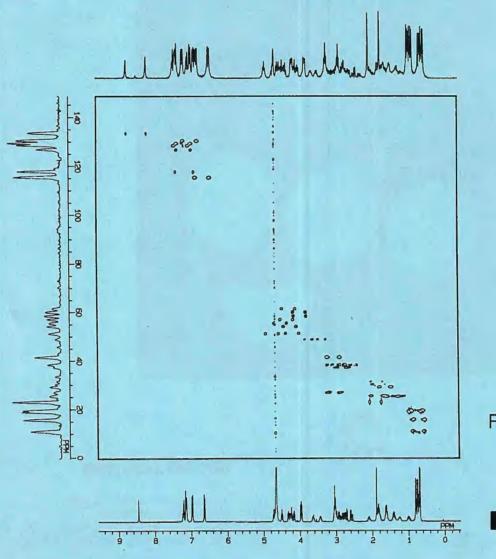
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